



17th International Young Scientist conference
“Developments in Optics and Communications” 2021



In-vivo diagnostics of skin malformations using multimodal RGB imaging

Laura Dambite



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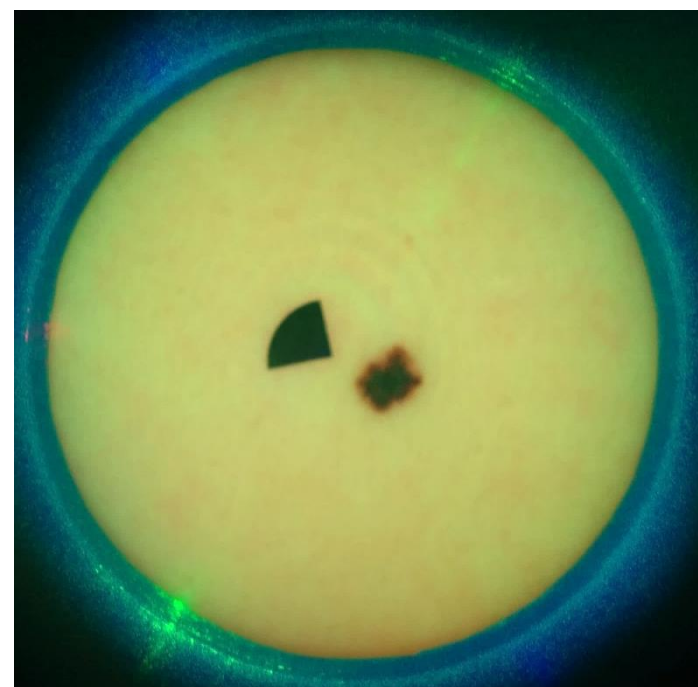


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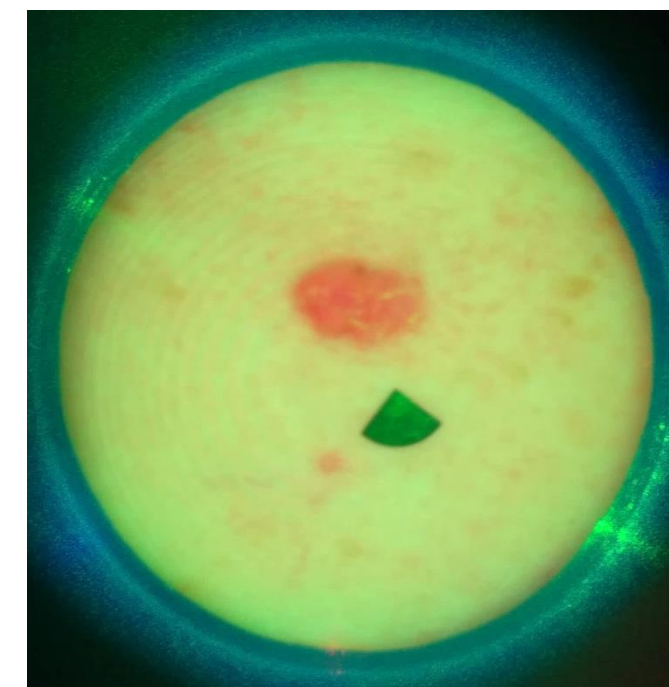
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Melanoma

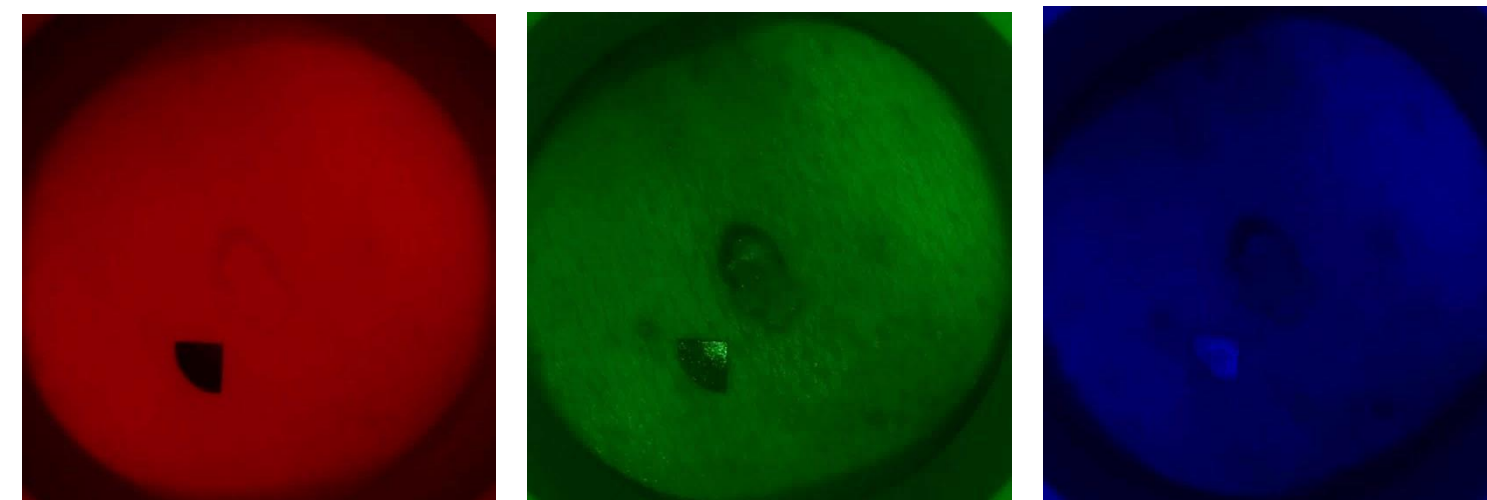


Laser
device

Basal cell carcinoma



LED
device

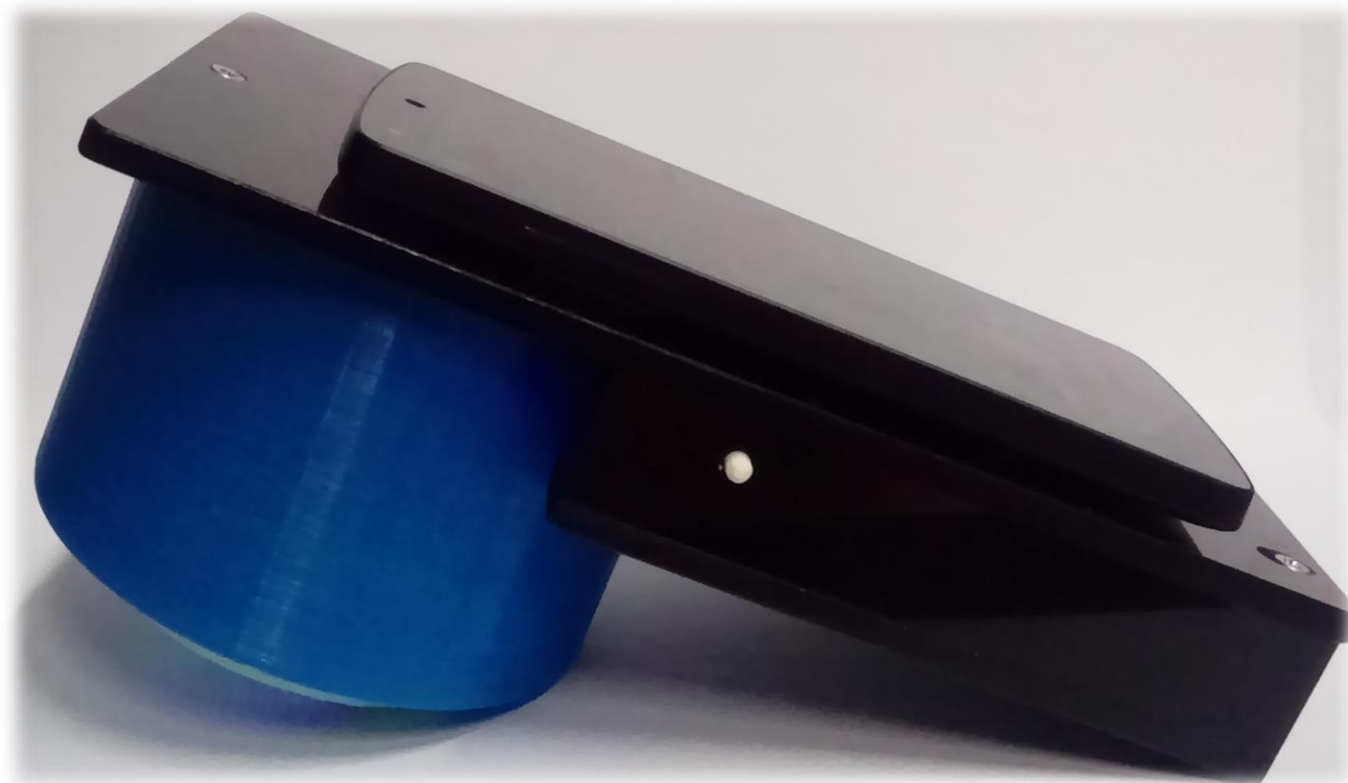


Suspicious skin malformations such as melanoma and basal cell carcinoma requires a histological examination that is precise, but invasive.



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Our devices



Multispectral laser device
(448 nm, 532 nm, 659 nm)



Multispectral LED device
(460 nm, 535 nm, 663 nm)



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Chromophore concentration calculation

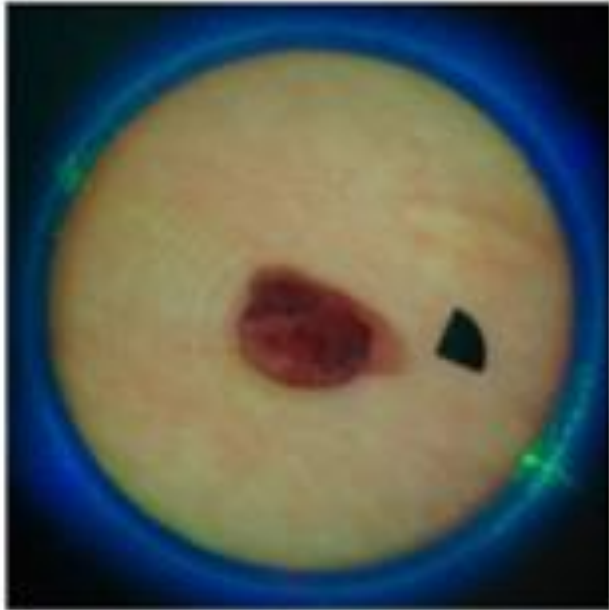
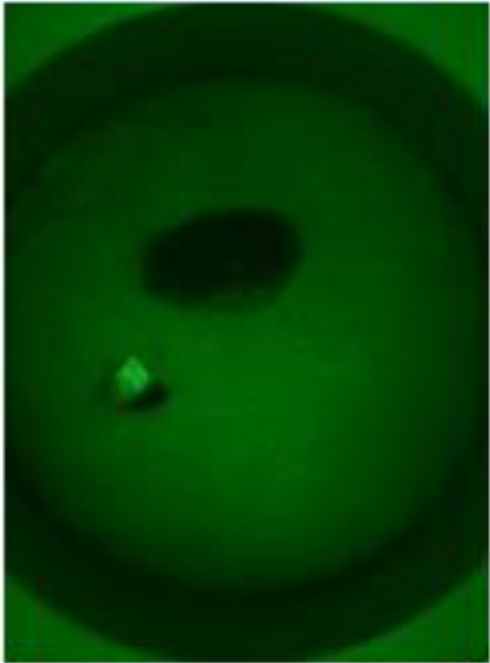
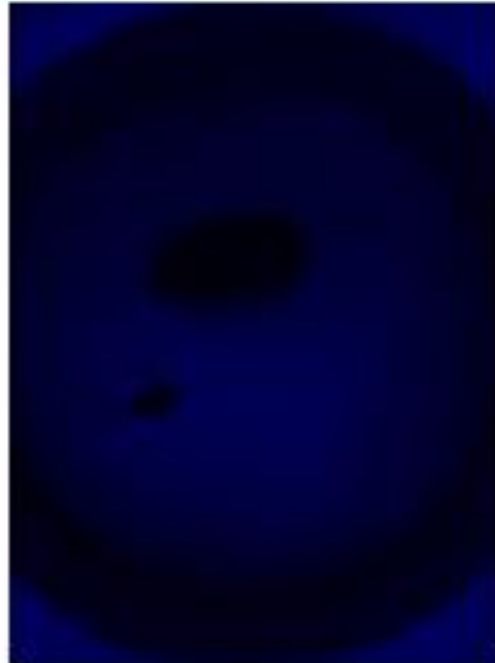
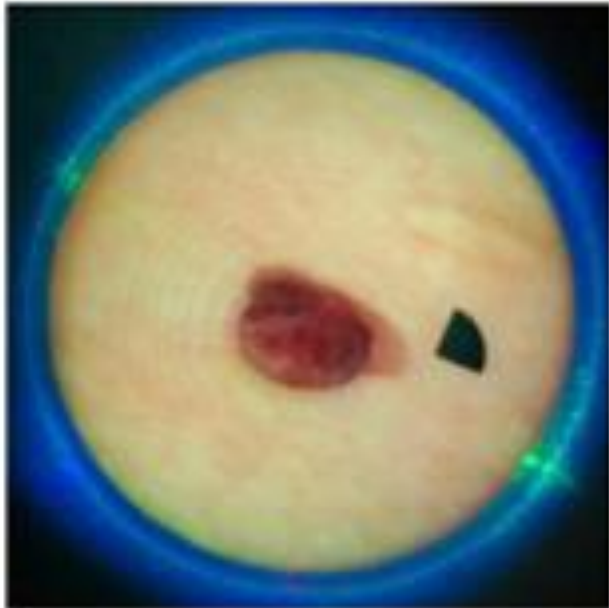
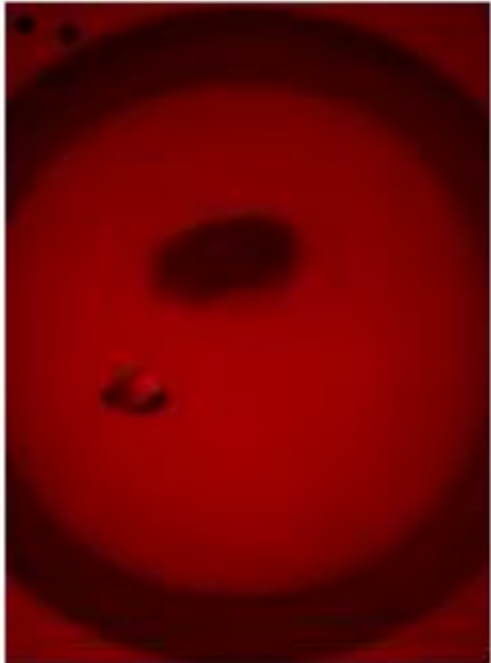
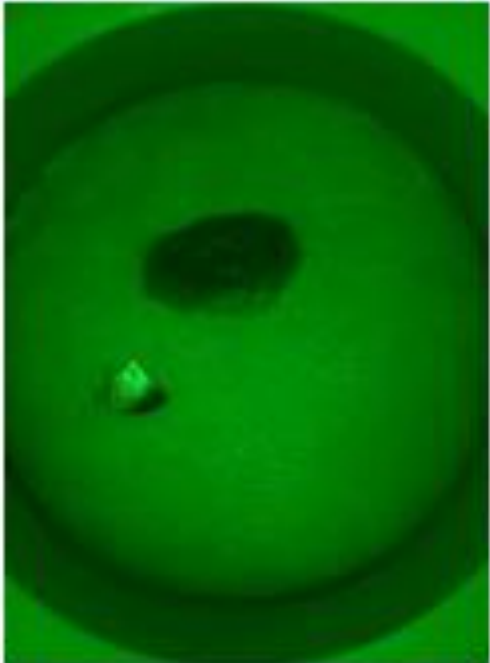
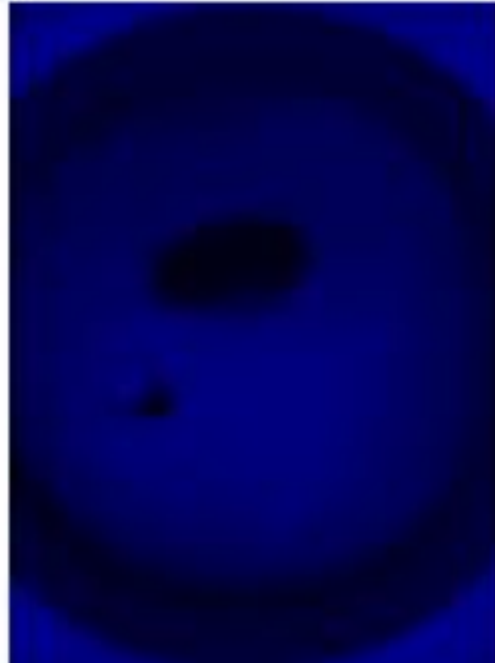


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Subtracts noise
from images

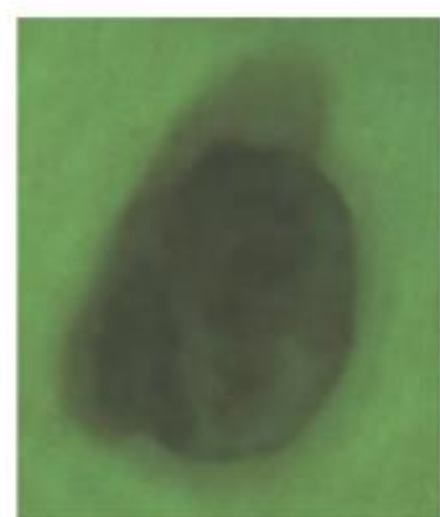


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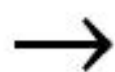
	Laser device	LED device		
With noise				
Without noise				



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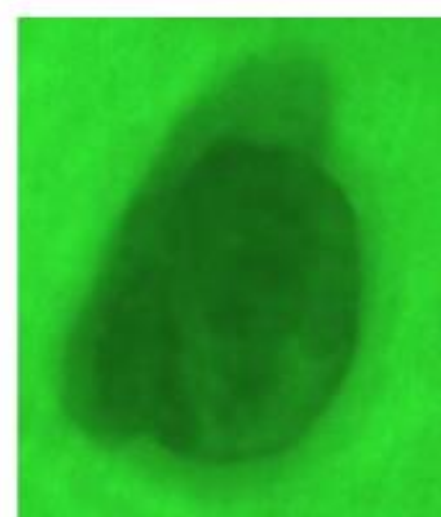


All lasers



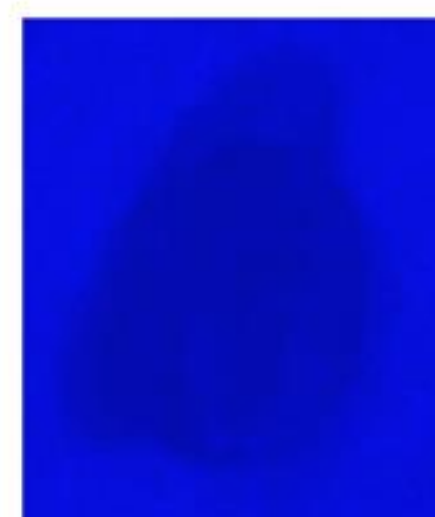
659 nm

+



532 nm

+



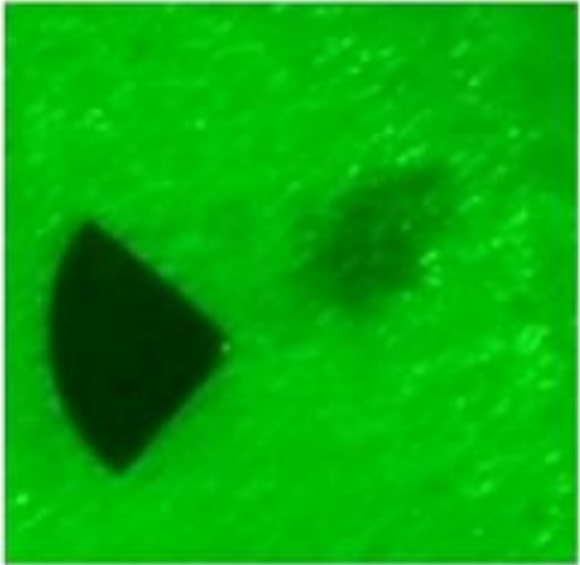
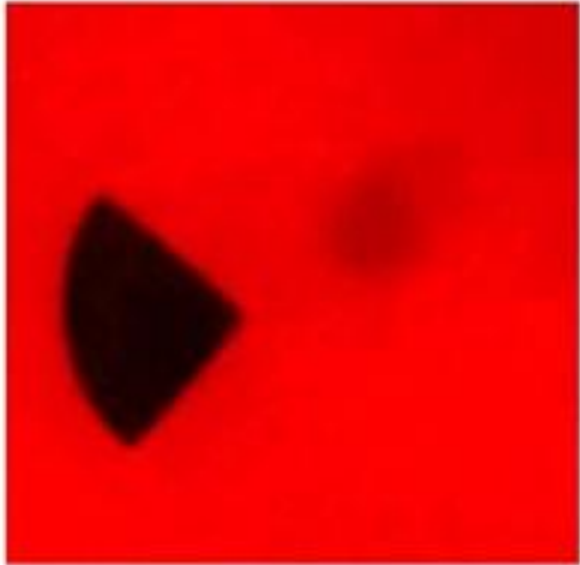
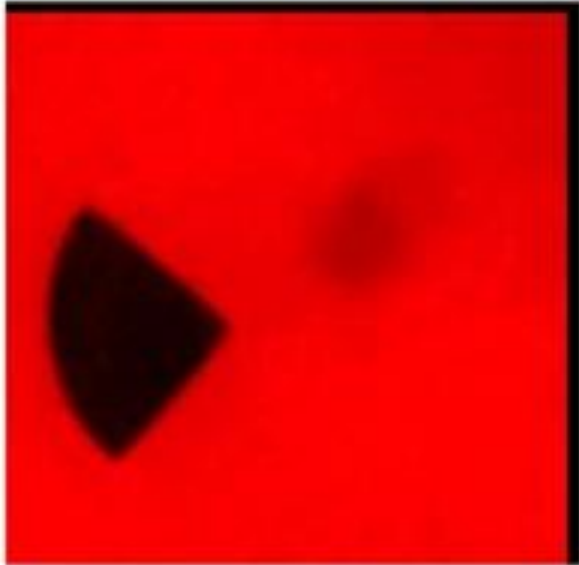
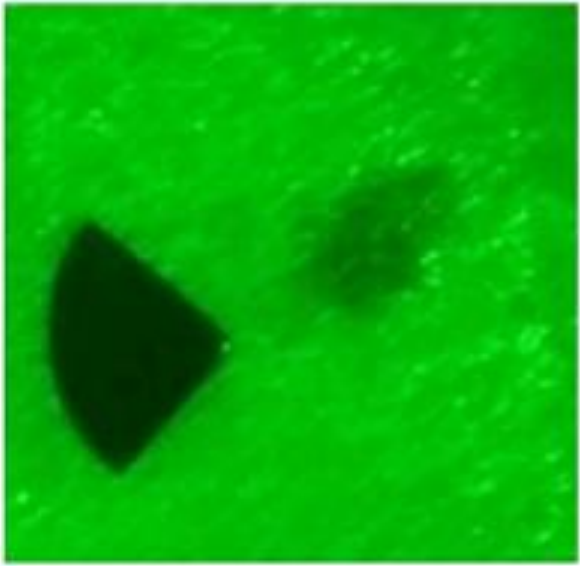
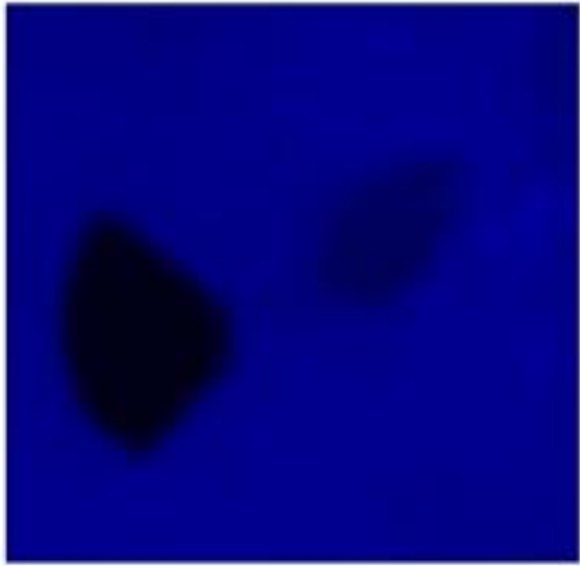
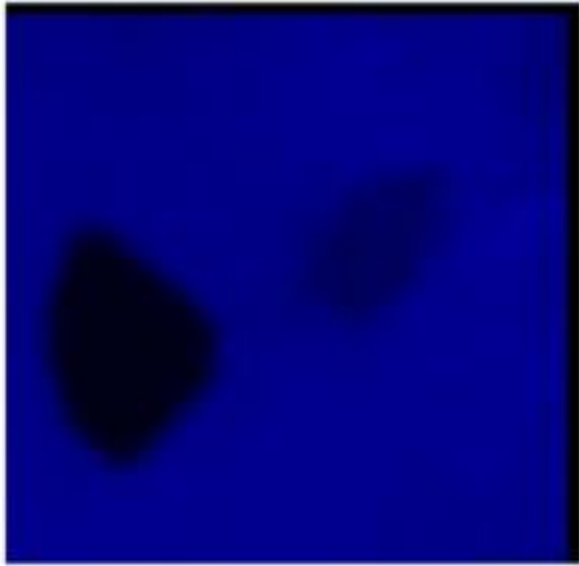
448 nm

Using the RGB
crosstalk correction
algorithm, three
images – one for
each wavelength –
are extracted in
laser device case



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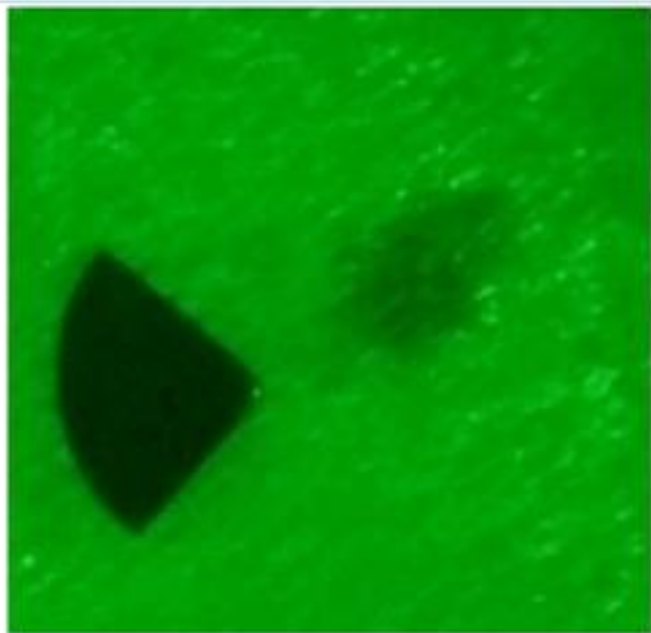
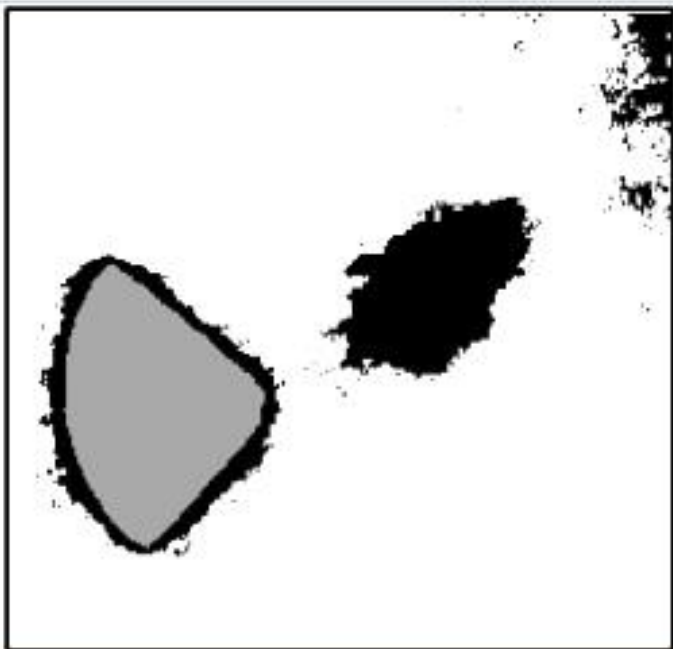
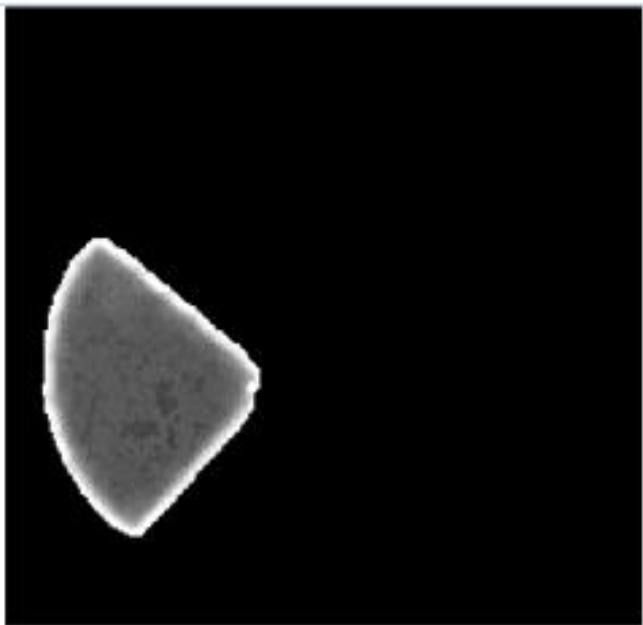
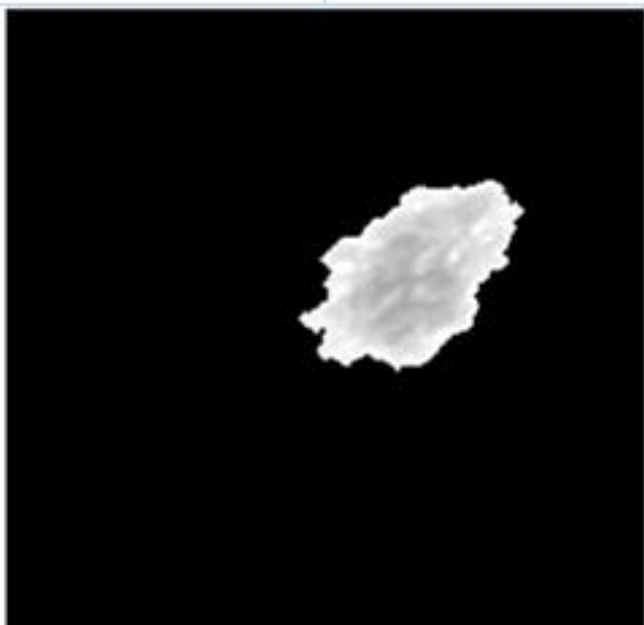
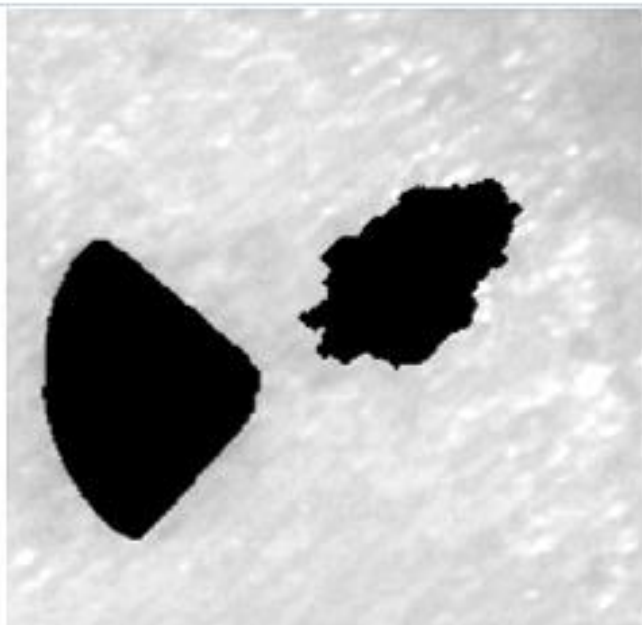


Green LED	Red LED	Stabilized red LED
		
Green LED	Blue LED	Stabilized blue LED
		

Using a stabilization algorithm and black marker, the images are combined to prevent motion artefacts in LED device case

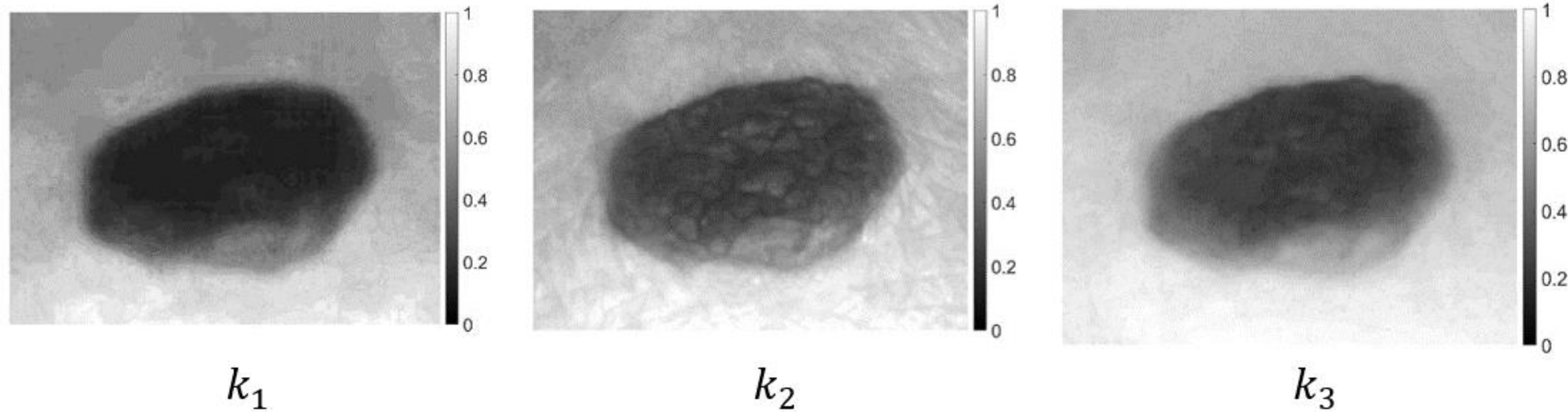




			
Green image		Segmented image	
			
Separated black marker	Separated pathology	Separated healthy skin	

Images are segmented to separate healthy skin, pathology and black marker for LED device case, and healthy skin and pathology for laser device case





$$k_i = \frac{I_i}{I_{0i}}$$

I_i – intensity of diffused reflected light from the skin pathology,
 I_{0i} – intensity of diffused reflected light from the healthy skin,

Calculate the mean values from the healthy skin area for each of the wavelengths and divide the area of interest by them to obtain three attenuation coefficients k_i





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Algorithms for skin chromophore mapping

Beer-Lambert law:

$$I = I_0 e^{-\mu_a \cdot l}$$

I – intensity of diffused reflected light from the skin malformation,

I_0 – intensity of diffused reflected light from the healthy skin,

l –photon mean path length in the skin

μ_a – absorption coefficient

First approach

Positive chromophore
concentration values
1,4%



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$$\left\{ \begin{array}{l} c_{\text{Mel}} \cdot \varepsilon_{\text{Mel}}(\lambda_1) + c_{\text{Oks}} \cdot \varepsilon_{\text{Oks}}(\lambda_1) + c_{\text{Deoks}} \cdot \varepsilon_{\text{Deoks}}(\lambda_1) = \frac{\ln \frac{I_0(\lambda_1)}{I(\lambda_1)}}{2,303 \cdot l(\lambda_1)} \\ c_{\text{Mel}} \cdot \varepsilon_{\text{Mel}}(\lambda_2) + c_{\text{Oks}} \cdot \varepsilon_{\text{Oks}}(\lambda_2) + c_{\text{Deoks}} \cdot \varepsilon_{\text{Deoks}}(\lambda_2) = \frac{\ln \frac{I_0(\lambda_2)}{I(\lambda_2)}}{2,303 \cdot l(\lambda_2)} \\ c_{\text{Mel}} \cdot \varepsilon_{\text{Mel}}(\lambda_3) + c_{\text{Oks}} \cdot \varepsilon_{\text{Oks}}(\lambda_3) + c_{\text{Deoks}} \cdot \varepsilon_{\text{Deoks}}(\lambda_3) = \frac{\ln \frac{I_0(\lambda_3)}{I(\lambda_3)}}{2,303 \cdot l(\lambda_3)} \end{array} \right.$$

Mel – melanin, *Oks* – oxyhemoglobin, *Deoks* – deoksihemoglobin,

ε – extinction coefficient, c – chromophore concentration,

I – intensity of diffused reflected light from the skin malformation,

I_0 – intensity of diffused reflected light from the healthy skin,

l – photon mean path length in the skin

$$k_i = \frac{I_i}{I_{0i}}$$

k_i – attenuation coefficient

Second approach

Positive chromophore concentration values
0,03%



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$$\begin{cases} c_{\text{Mel}} \cdot \varepsilon_{\text{Mel}}(\lambda_1) \cdot d_1 + (c_{\text{Oks}} \cdot \varepsilon_{\text{Oks}}(\lambda_1) + c_{\text{Deoks}} \cdot \varepsilon_{\text{Deoks}}(\lambda_1)) \cdot (1 - d_1) + z_1 = \frac{\ln \frac{I_0(\lambda_1)}{I(\lambda_1)}}{2,303 \cdot l(\lambda_1)} \\ c_{\text{Mel}} \cdot \varepsilon_{\text{Mel}}(\lambda_2) \cdot d_2 + (c_{\text{Oks}} \cdot \varepsilon_{\text{Oks}}(\lambda_2) + c_{\text{Deoks}} \cdot \varepsilon_{\text{Deoks}}(\lambda_2)) \cdot (1 - d_2) + z_2 = \frac{\ln \frac{I_0(\lambda_2)}{I(\lambda_2)}}{2,303 \cdot l(\lambda_2)} \\ c_{\text{Mel}} \cdot \varepsilon_{\text{Mel}}(\lambda_3) \cdot d_3 + (c_{\text{Oks}} \cdot \varepsilon_{\text{Oks}}(\lambda_3) + c_{\text{Deoks}} \cdot \varepsilon_{\text{Deoks}}(\lambda_3)) \cdot (1 - d_3) + z_3 = \frac{\ln \frac{I_0(\lambda_3)}{I(\lambda_3)}}{2,303 \cdot l(\lambda_3)} \end{cases}$$

Mel – melanin, *Oks* – oxyhemoglobin, *Deoks* – deoksihemoglobin,

ε – extinction coefficient, c – chromophore concentration,

I – intensity of diffused reflected light from the skin malformation,

I_0 – intensity of diffused reflected light from the healthy skin,

l – photon mean path length in the skin

$$k_i = \frac{I_i}{I_{0i}}$$

k_i – attenuation coefficient

d_i – part of the light that is absorbed in the epidermis at the wavelength λ_i ,

z_i – loss coefficient – describes the part of the light absorbed by other chromophores

Third approach

Positive chromophore concentration values
2,57%



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$$\begin{cases} c_{\text{Mel}} \cdot \varepsilon_{\text{Mel}}(\lambda_1) \sqrt{1 + \frac{\mu'_{s11}}{\mu_{a11}}} \cdot l_{11} + (c_{\text{Oks}} \cdot \varepsilon_{\text{Oks}}(\lambda_1) + c_{\text{Deoks}} \cdot \varepsilon_{\text{Deoks}}(\lambda_1)) \sqrt{1 + \frac{\mu'_{s12}}{\mu_{a12}}} \cdot l_{12} = \frac{\ln \frac{I_0(\lambda_1)}{I(\lambda_1)}}{\sqrt{3} \cdot 2,303} \\ c_{\text{Mel}} \cdot \varepsilon_{\text{Mel}}(\lambda_2) \sqrt{1 + \frac{\mu'_{s21}}{\mu_{a21}}} \cdot l_{21} + (c_{\text{Oks}} \cdot \varepsilon_{\text{Oks}}(\lambda_2) + c_{\text{Deoks}} \cdot \varepsilon_{\text{Deoks}}(\lambda_2)) \sqrt{1 + \frac{\mu'_{s22}}{\mu_{a22}}} \cdot l_{22} = \frac{\ln \frac{I_0(\lambda_2)}{I(\lambda_2)}}{\sqrt{3} \cdot 2,303} \\ c_{\text{Mel}} \cdot \varepsilon_{\text{Mel}}(\lambda_3) \sqrt{1 + \frac{\mu'_{s31}}{\mu_{a31}}} \cdot l_{31} + (c_{\text{Oks}} \cdot \varepsilon_{\text{Oks}}(\lambda_3) + c_{\text{Deoks}} \cdot \varepsilon_{\text{Deoks}}(\lambda_3)) \sqrt{1 + \frac{\mu'_{s32}}{\mu_{a32}}} \cdot l_{32} = \frac{\ln \frac{I_0(\lambda_3)}{I(\lambda_3)}}{\sqrt{3} \cdot 2,303} \end{cases}$$

Mel – melanin, *Oks* – oxyhemoglobin, *Deoks* – deoksihemoglobin,

ε – extinction coefficient, c – chromophore concentration,

I – intensity of diffused reflected light from the skin malformation,

I_0 – intensity of diffused reflected light from the healthy skin,

l –photon mean path length in the skin

μ_a – absorption coefficient

μ'_s – reduced scattering coefficient

Fourth approach

Positive chromophore concentration values 1,35%



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$$\begin{cases} c_{\text{Mel}} \cdot \varepsilon_{\text{Mel}}(\lambda_1) \sqrt{1 + \frac{\mu'_{s11}}{\mu_{a11}}} \cdot l_{11} + (c_{\text{Oks}} \cdot \varepsilon_{\text{Oks}}(\lambda_1) + c_{\text{Deoks}} \cdot \varepsilon_{\text{Deoks}}(\lambda_1)) \cdot B_1 = \frac{\ln \frac{I_0(\lambda_1) \cdot Nn_1}{I(\lambda_1)}}{\sqrt{3} \cdot 4,606} \\ c_{\text{Mel}} \cdot \varepsilon_{\text{Mel}}(\lambda_2) \sqrt{1 + \frac{\mu'_{s21}}{\mu_{a21}}} \cdot l_{21} + (c_{\text{Oks}} \cdot \varepsilon_{\text{Oks}}(\lambda_2) + c_{\text{Deoks}} \cdot \varepsilon_{\text{Deoks}}(\lambda_2)) \cdot B_2 = \frac{\ln \frac{I_0(\lambda_2) \cdot Nn_2}{I(\lambda_2)}}{\sqrt{3} \cdot 4,606} \\ c_{\text{Mel}} \cdot \varepsilon_{\text{Mel}}(\lambda_3) \sqrt{1 + \frac{\mu'_{s31}}{\mu_{a31}}} \cdot l_{31} + (c_{\text{Oks}} \cdot \varepsilon_{\text{Oks}}(\lambda_3) + c_{\text{Deoks}} \cdot \varepsilon_{\text{Deoks}}(\lambda_3)) \cdot B_3 = \frac{\ln \frac{I_0(\lambda_3) \cdot Nn_3}{I(\lambda_3)}}{\sqrt{3} \cdot 4,606} \end{cases}$$

$$B_i = \sum_{n=2}^5 \sqrt{1 + \frac{\mu'_{sin}}{\mu_{ain}}} \cdot l_{in}$$

Mel – melanin, *Oks* – oxyhemoglobin, *Deoks* – deoksihemoglobin,

ε – extinction coefficient, c – chromophore concentration,

I – intensity of diffused reflected light from the skin malformation,

I_0 – intensity of diffused reflected light from the healthy skin,

l –photon mean path length in the skin

μ_a – absorption coefficient

μ'_s – reduced scattering coefficient

Nn – interlayer reflection coefficient



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Results

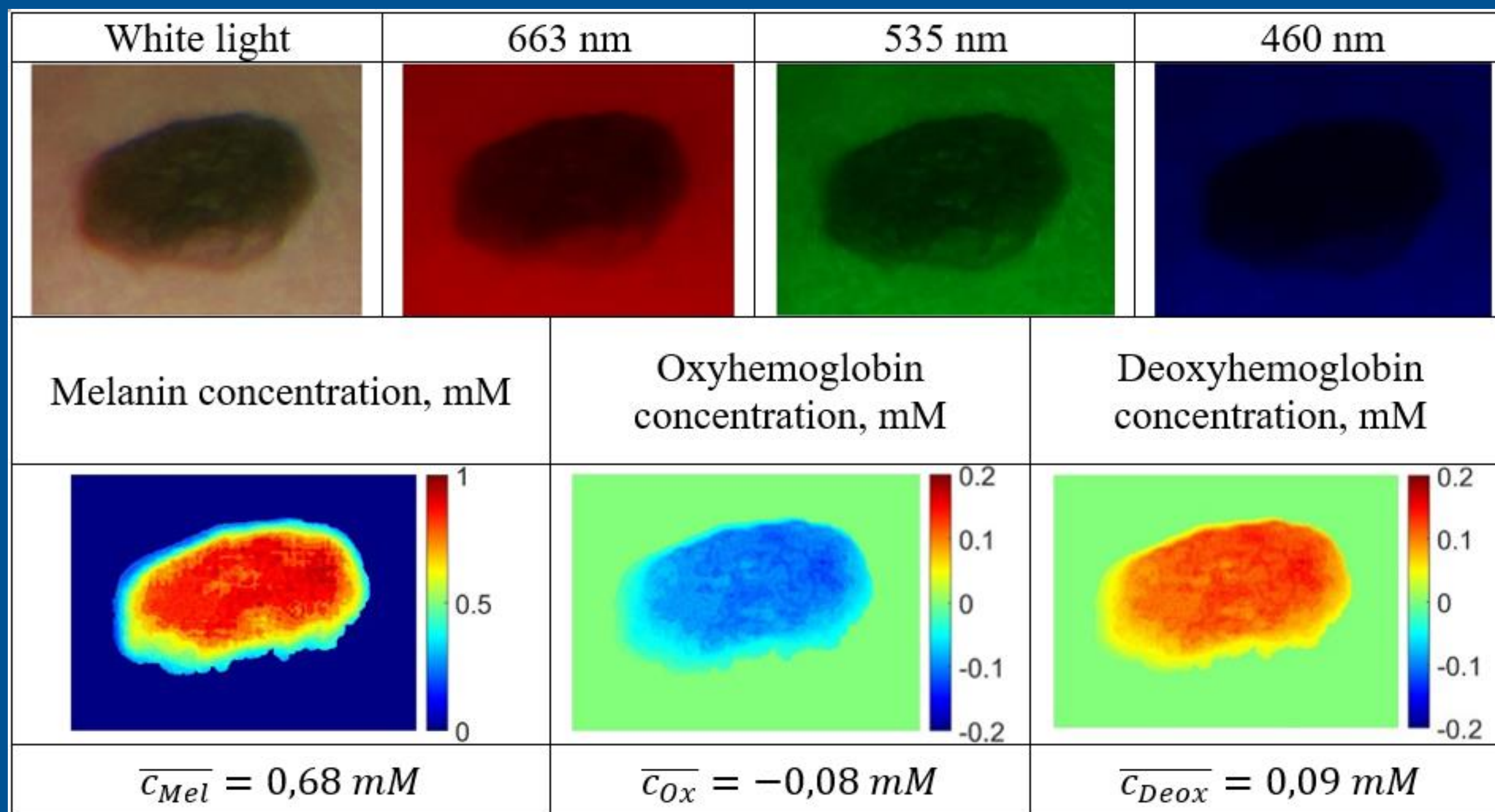


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Chromophore maps

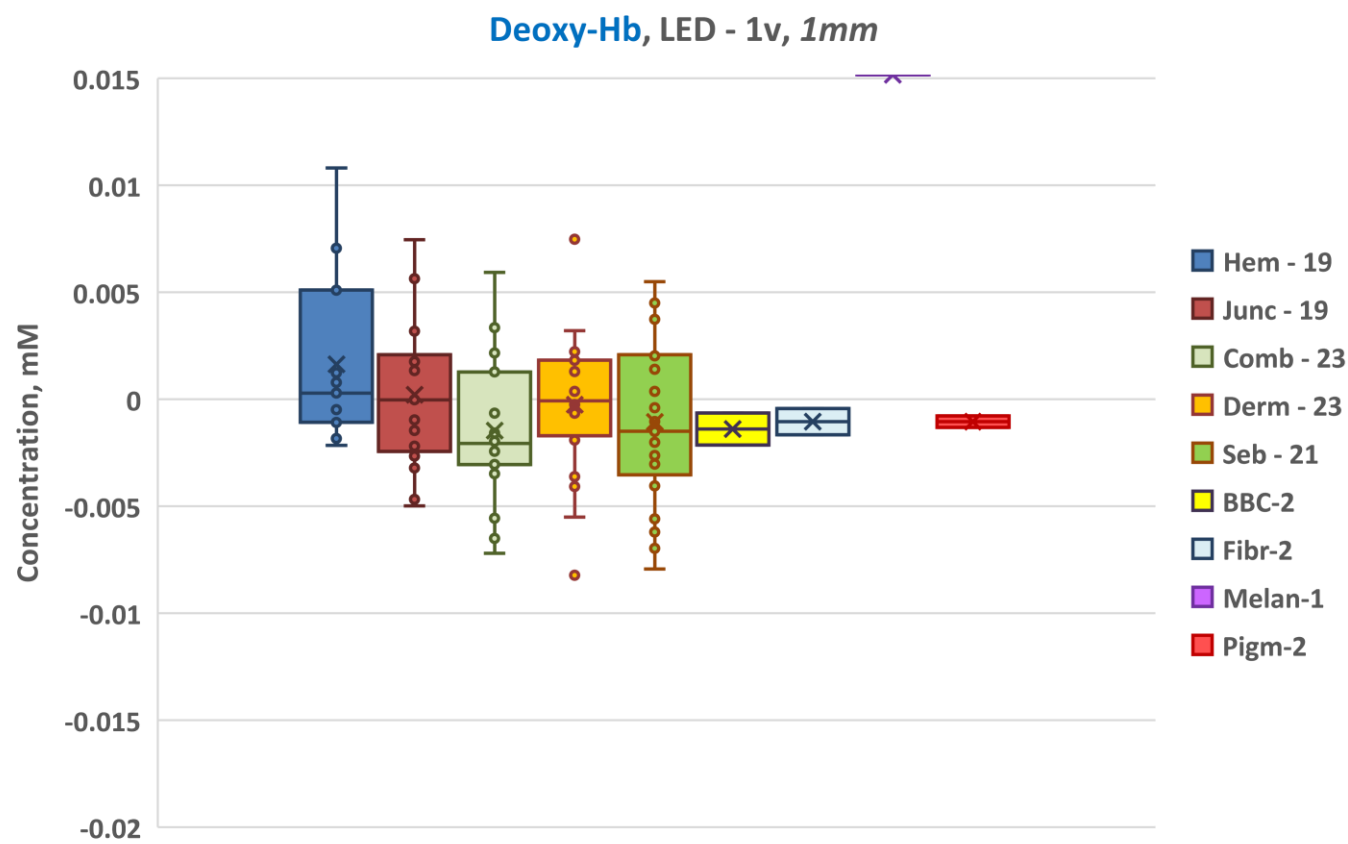
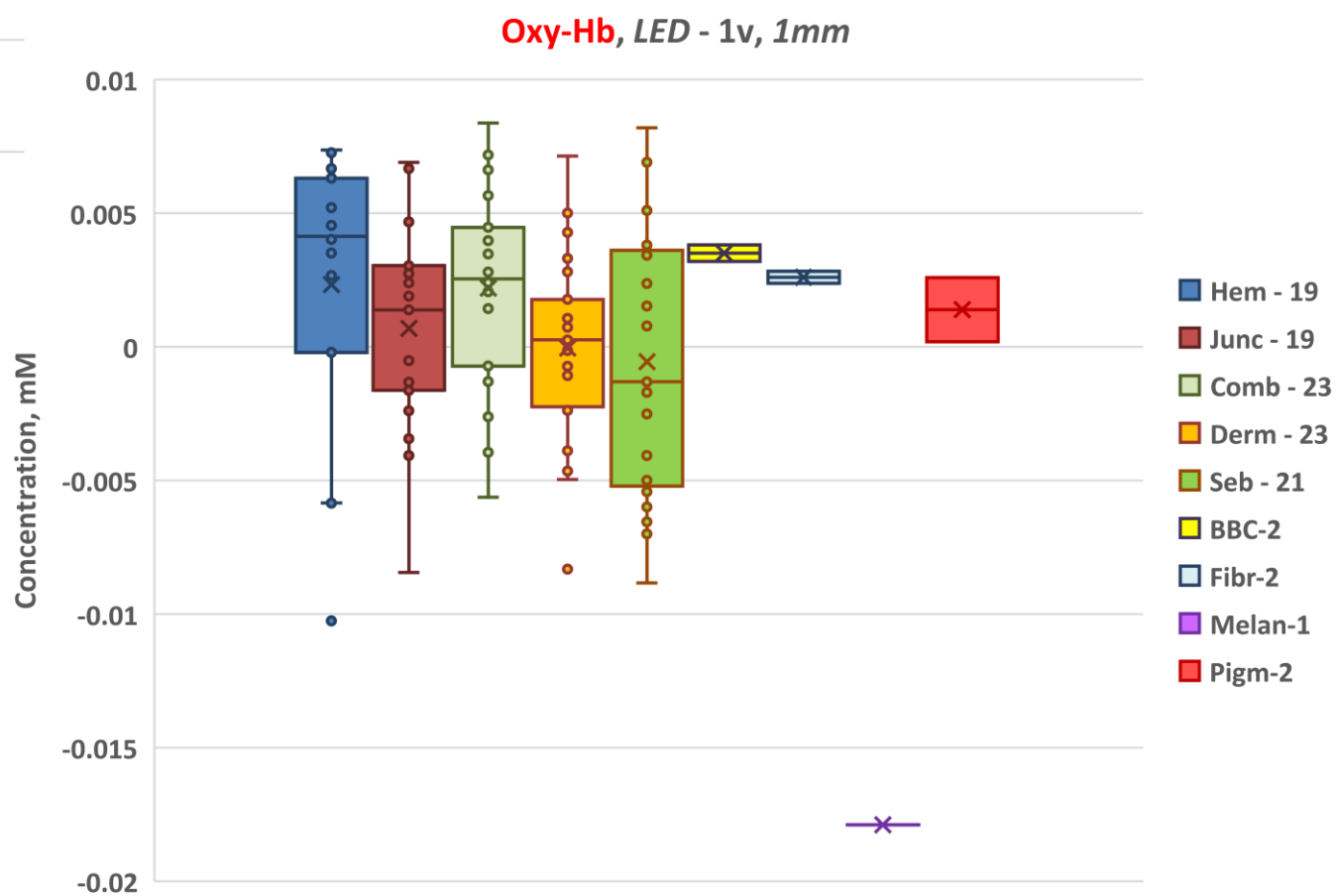
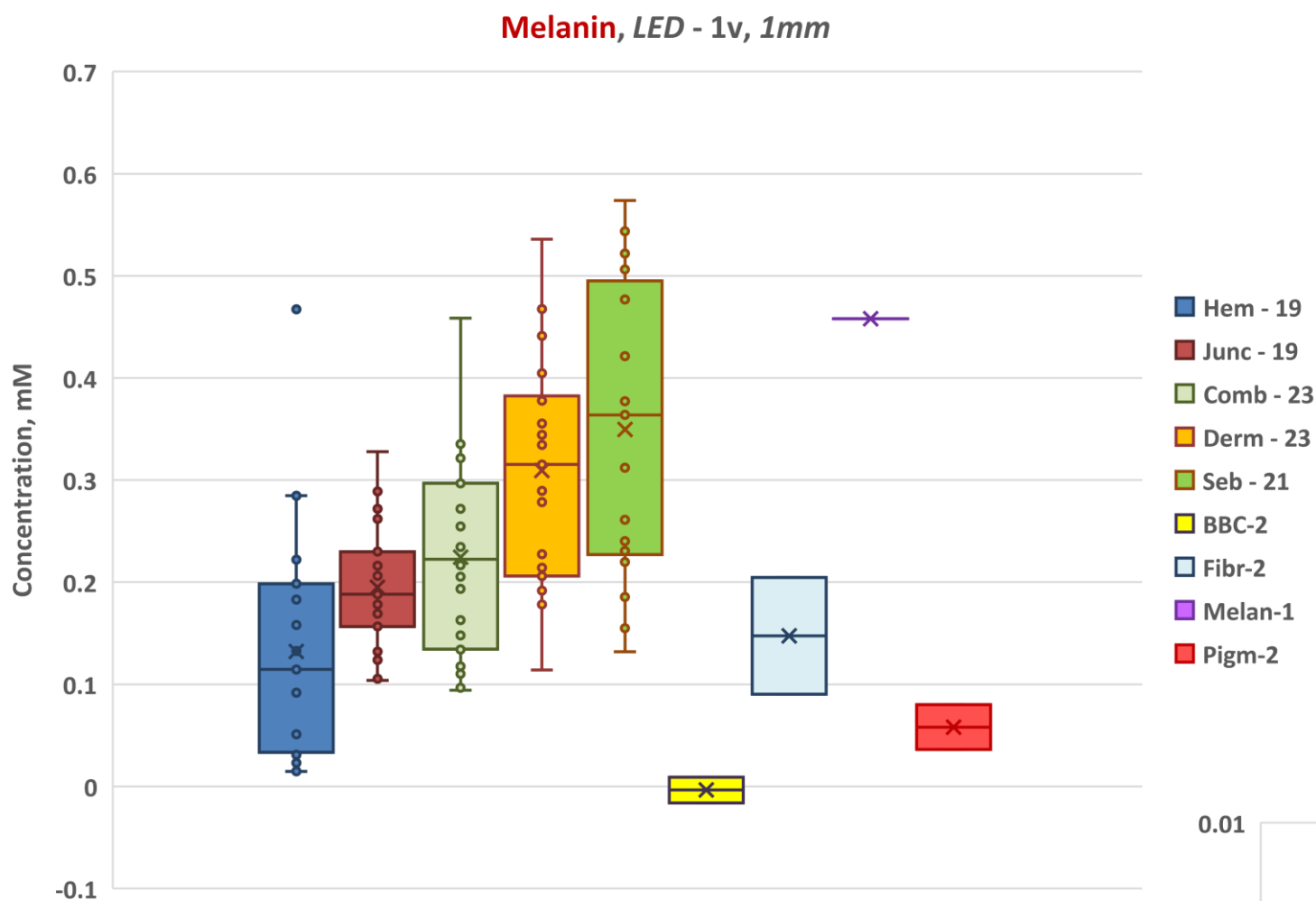


First approach for *LED* images



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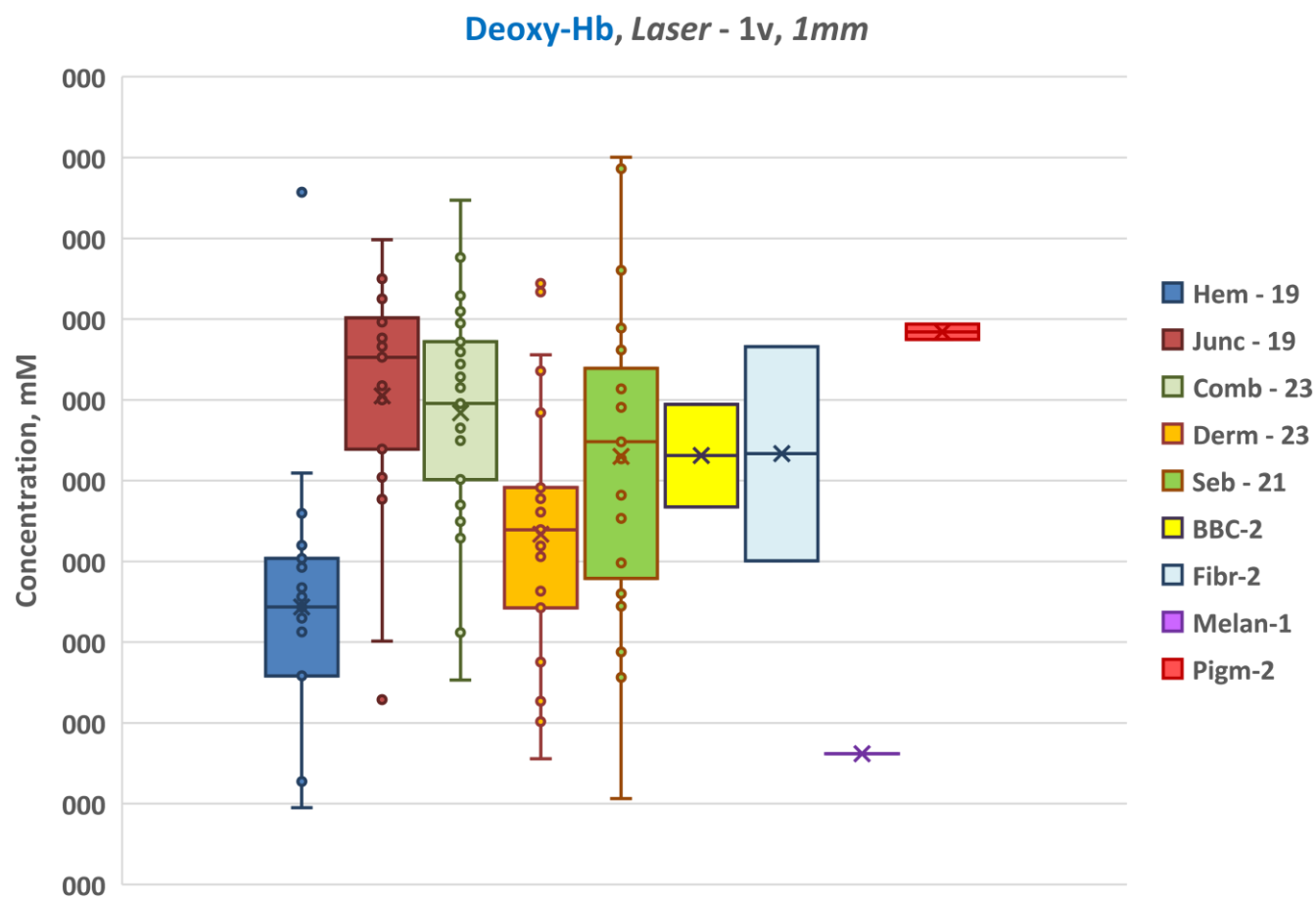
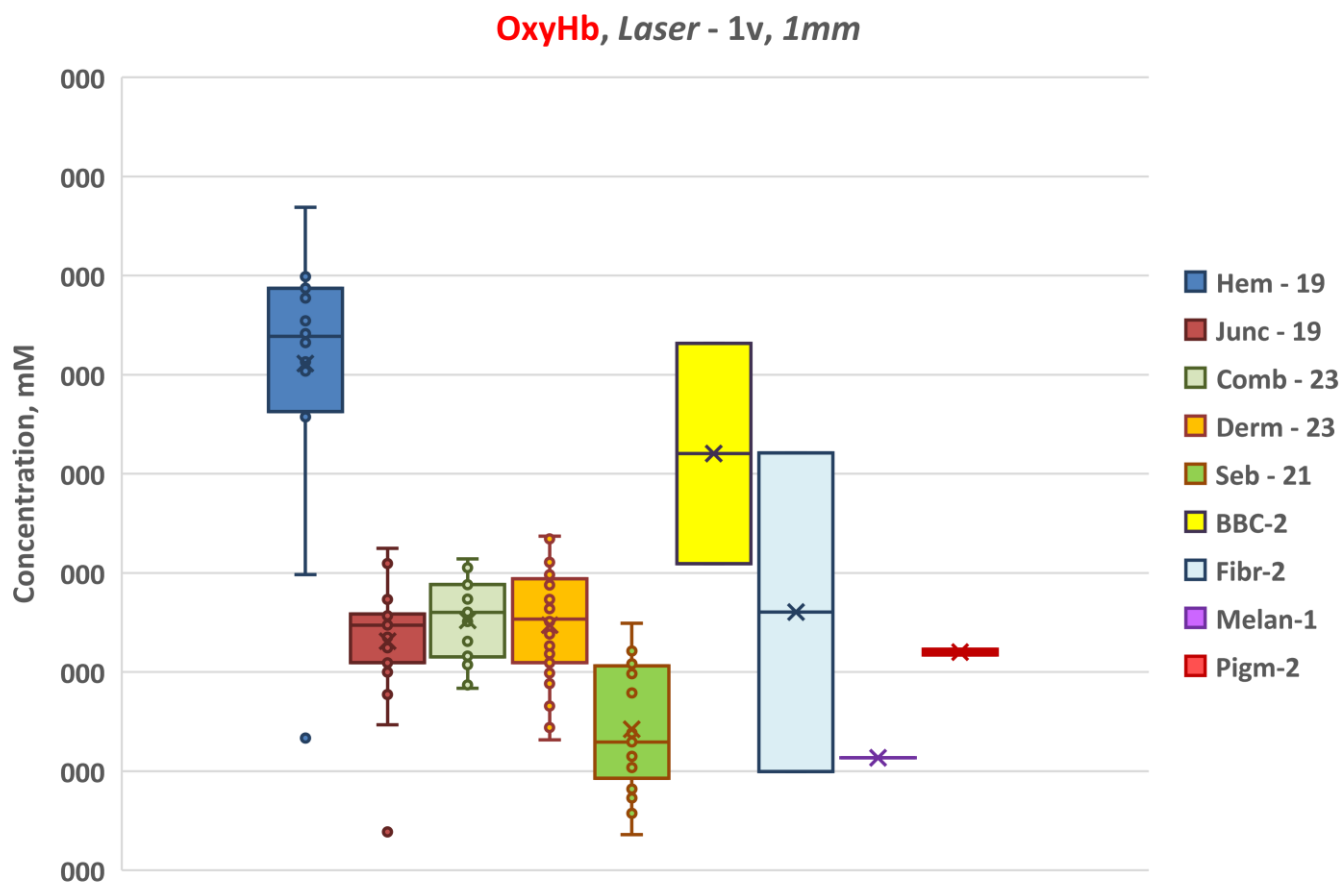
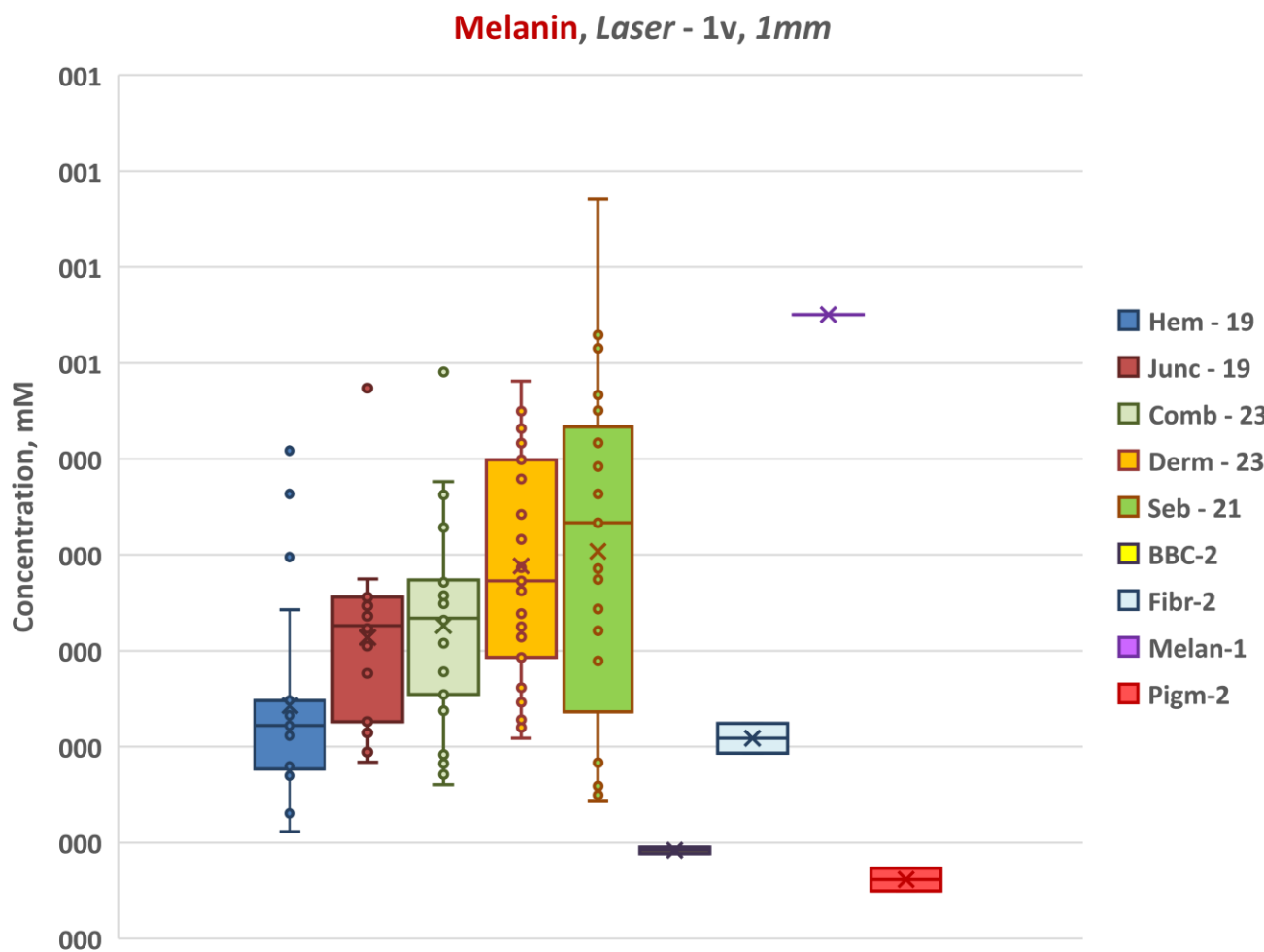


First approach for *Laser* images



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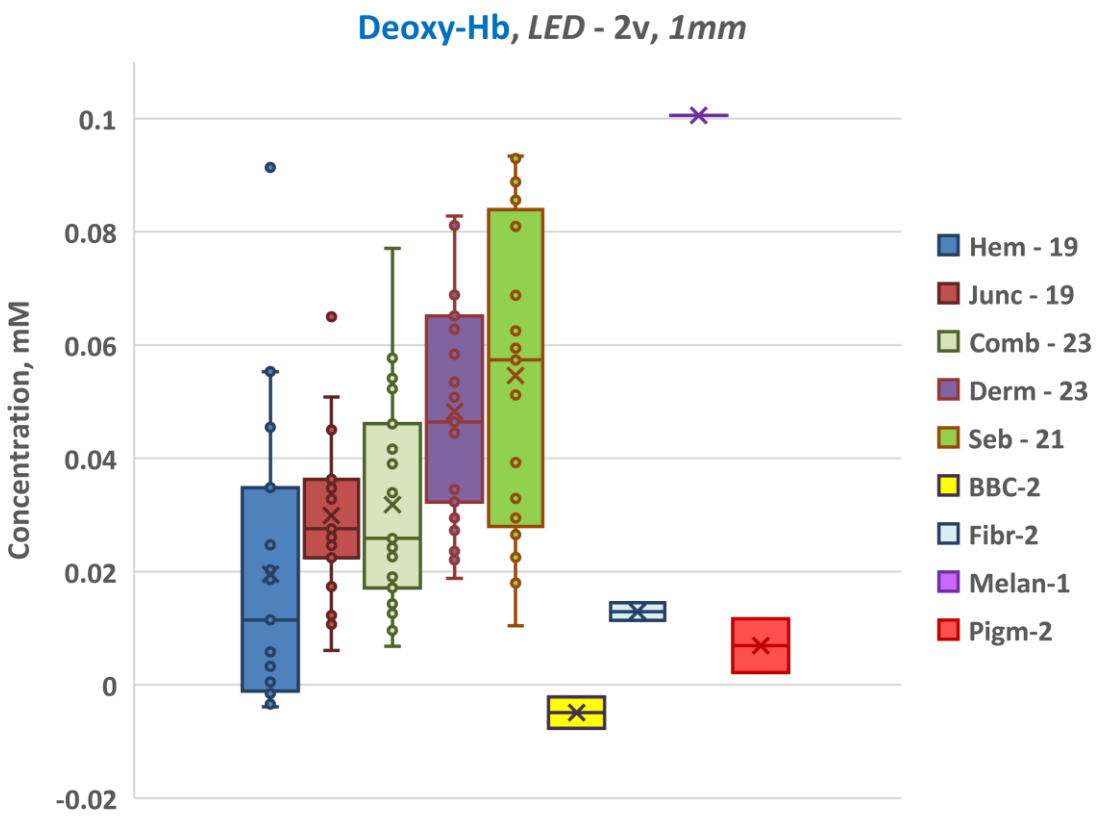
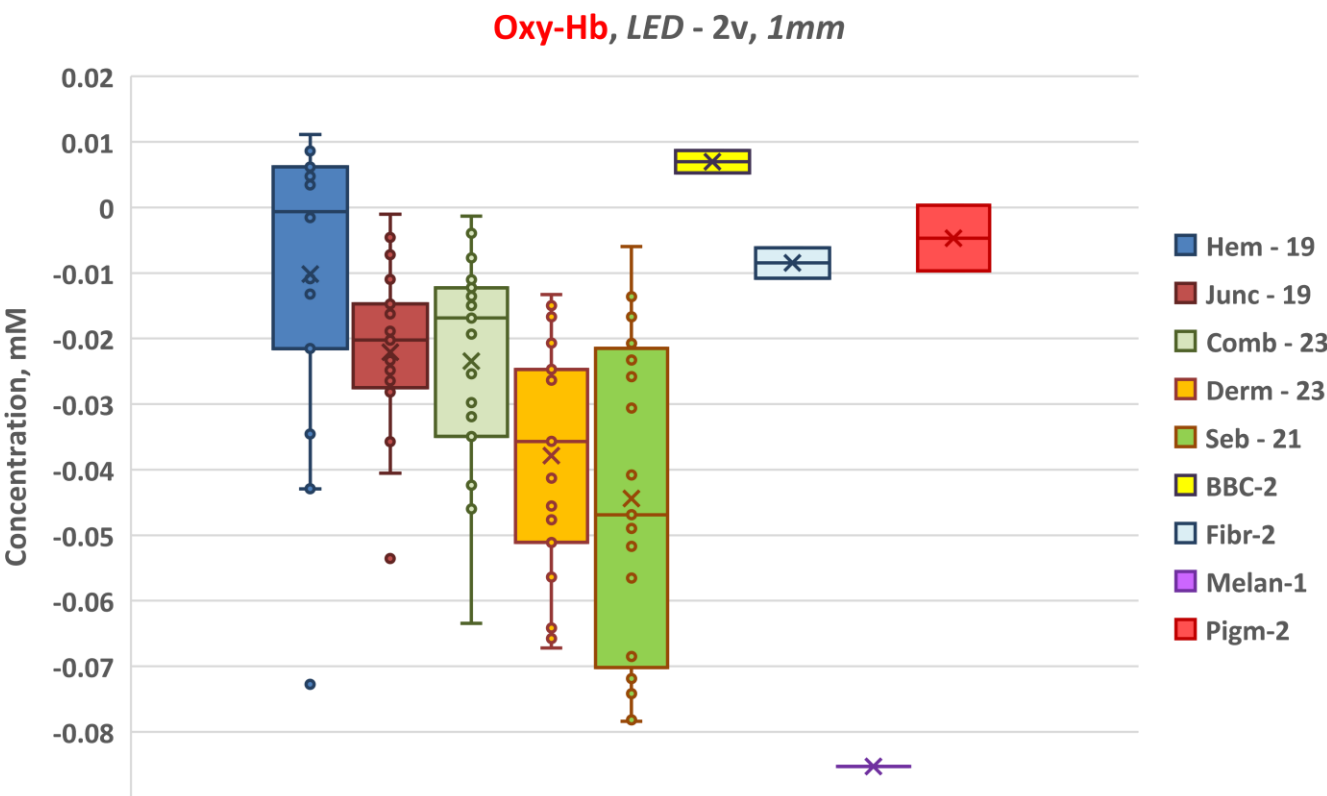
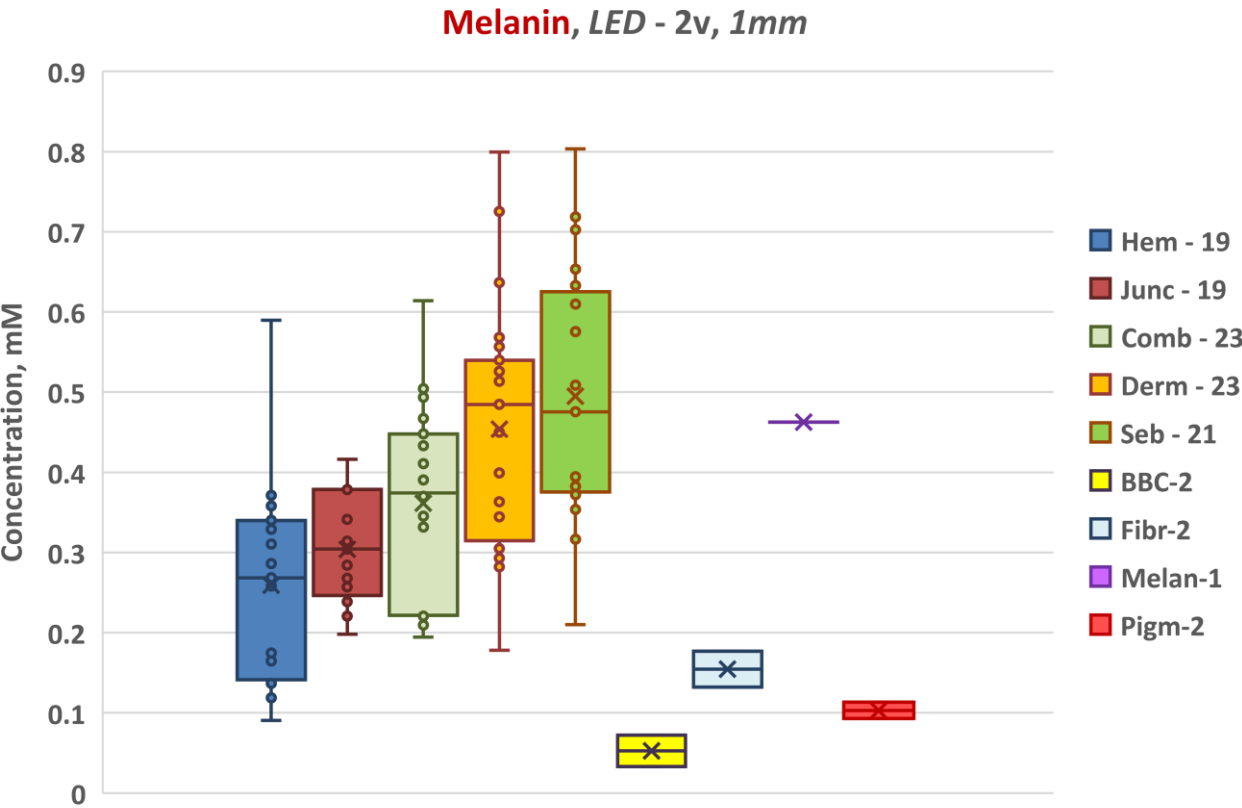


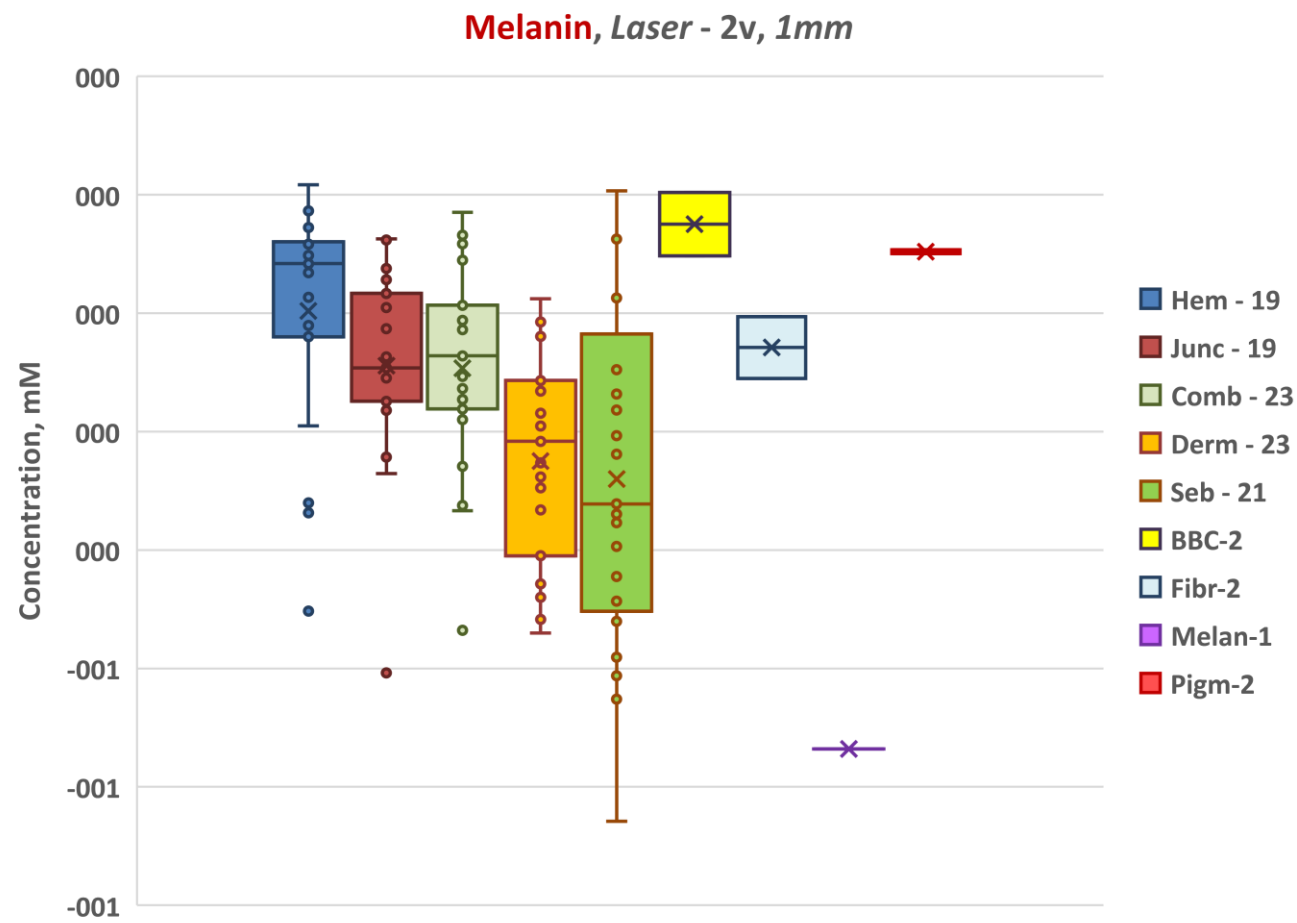


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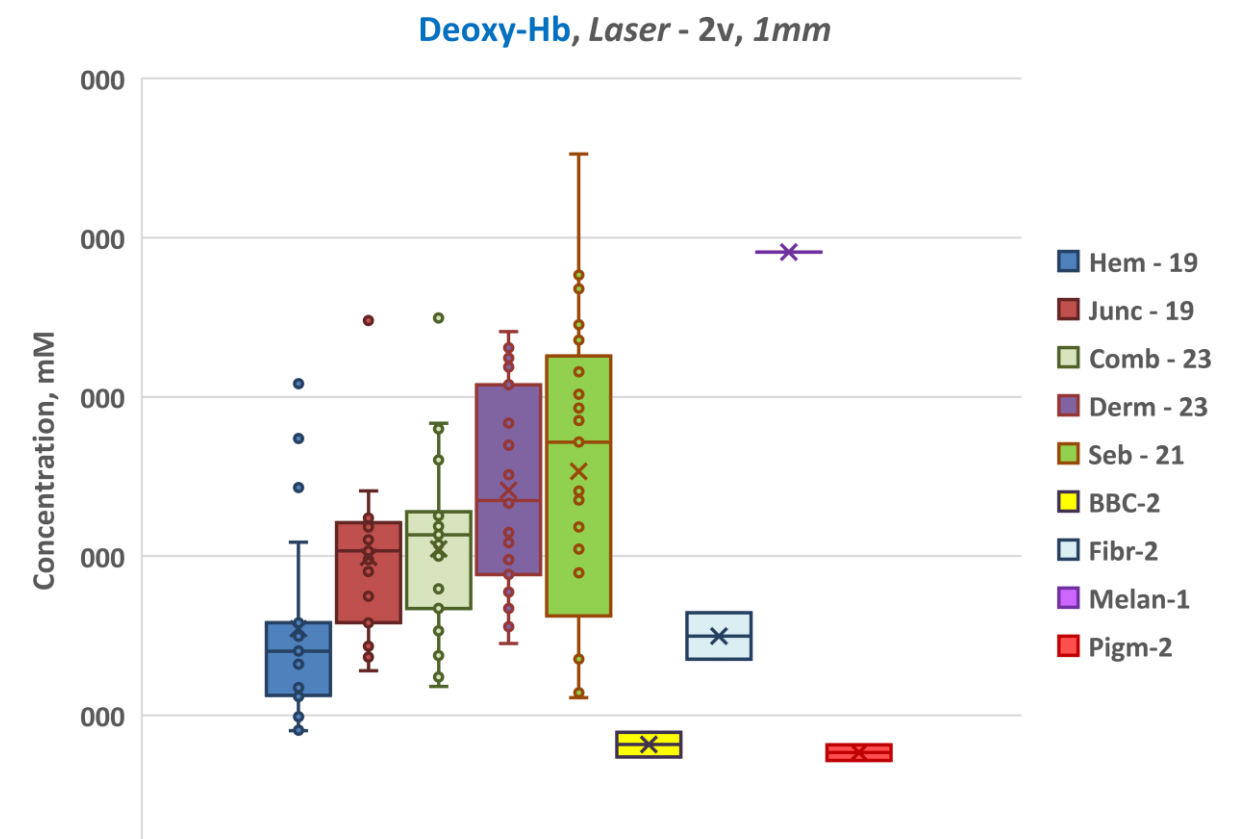
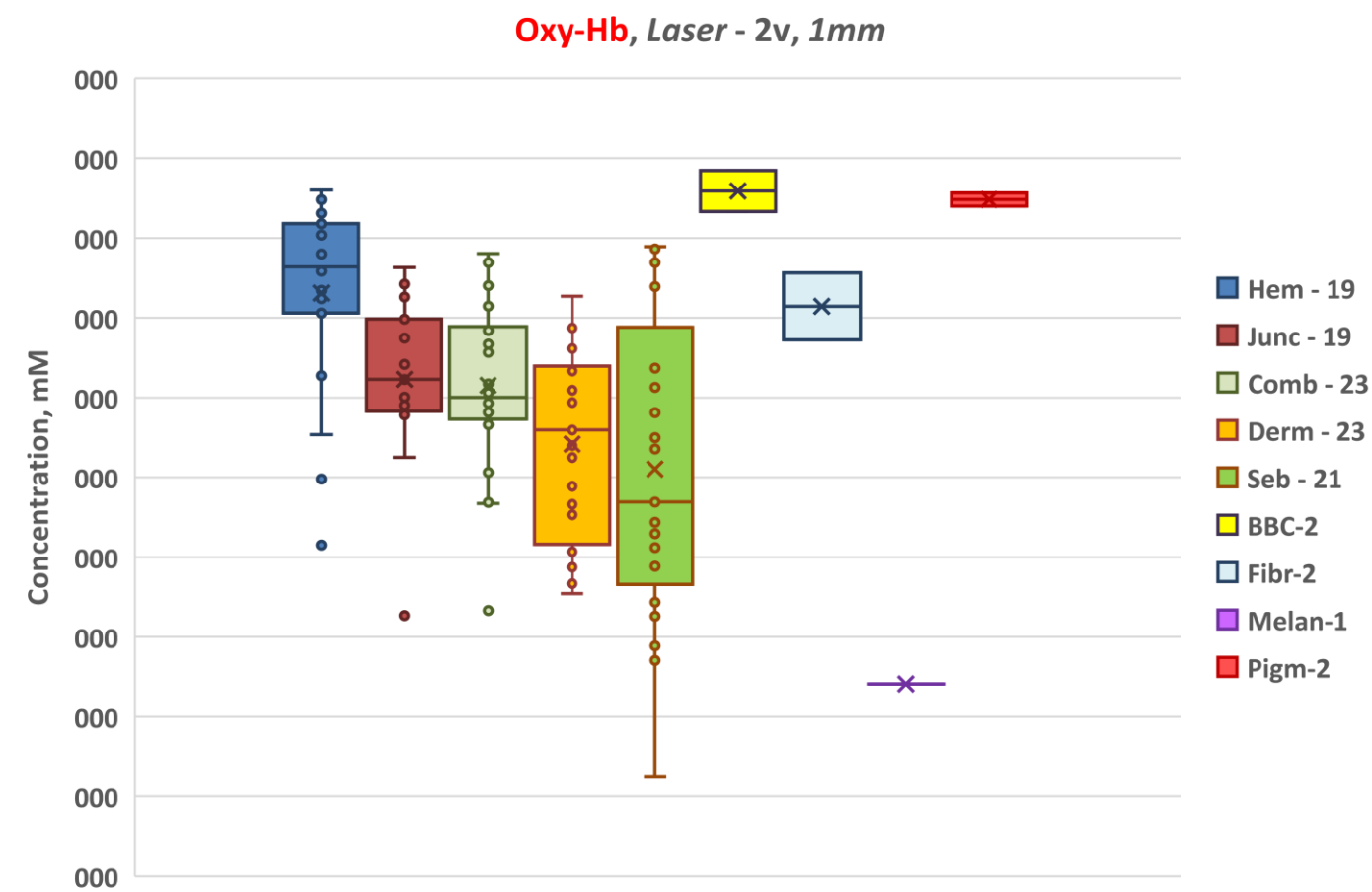
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Second approach for *LED* images





Second approach for *Laser* images

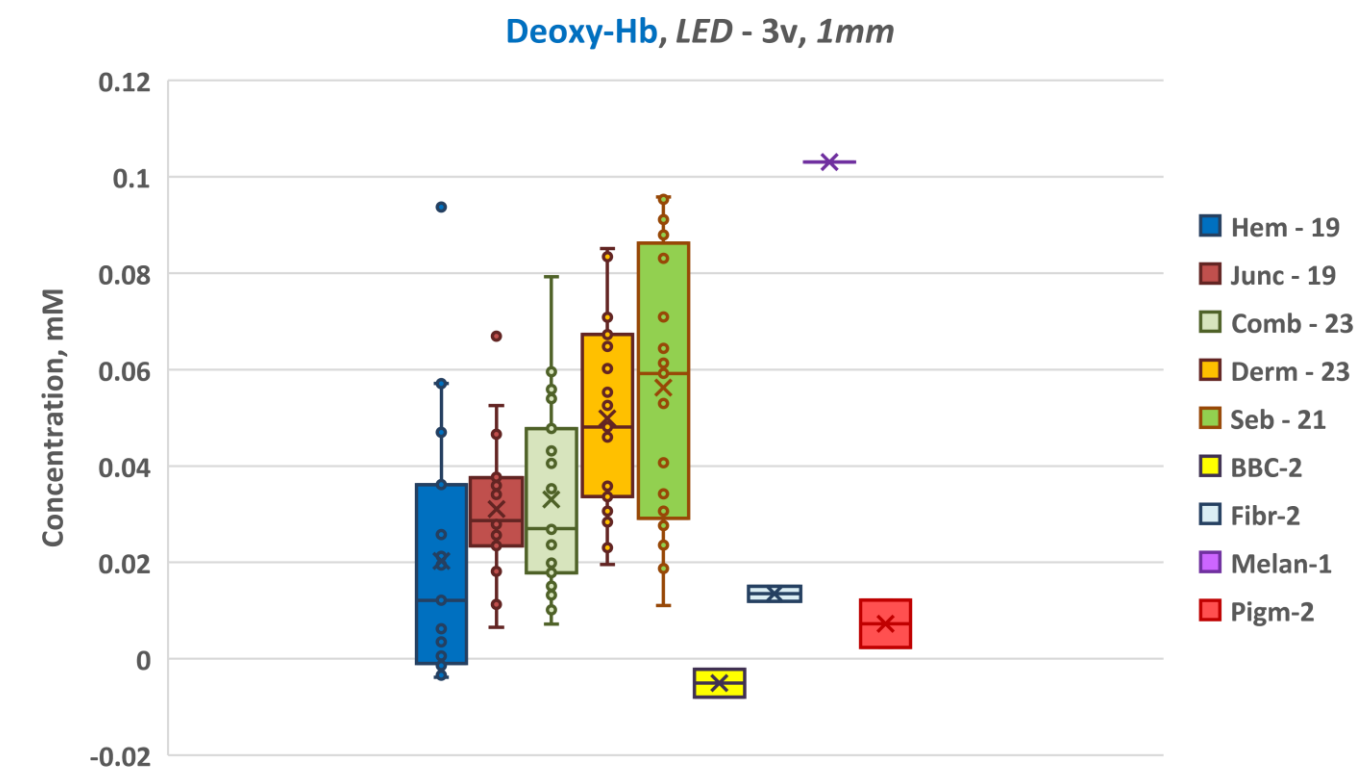
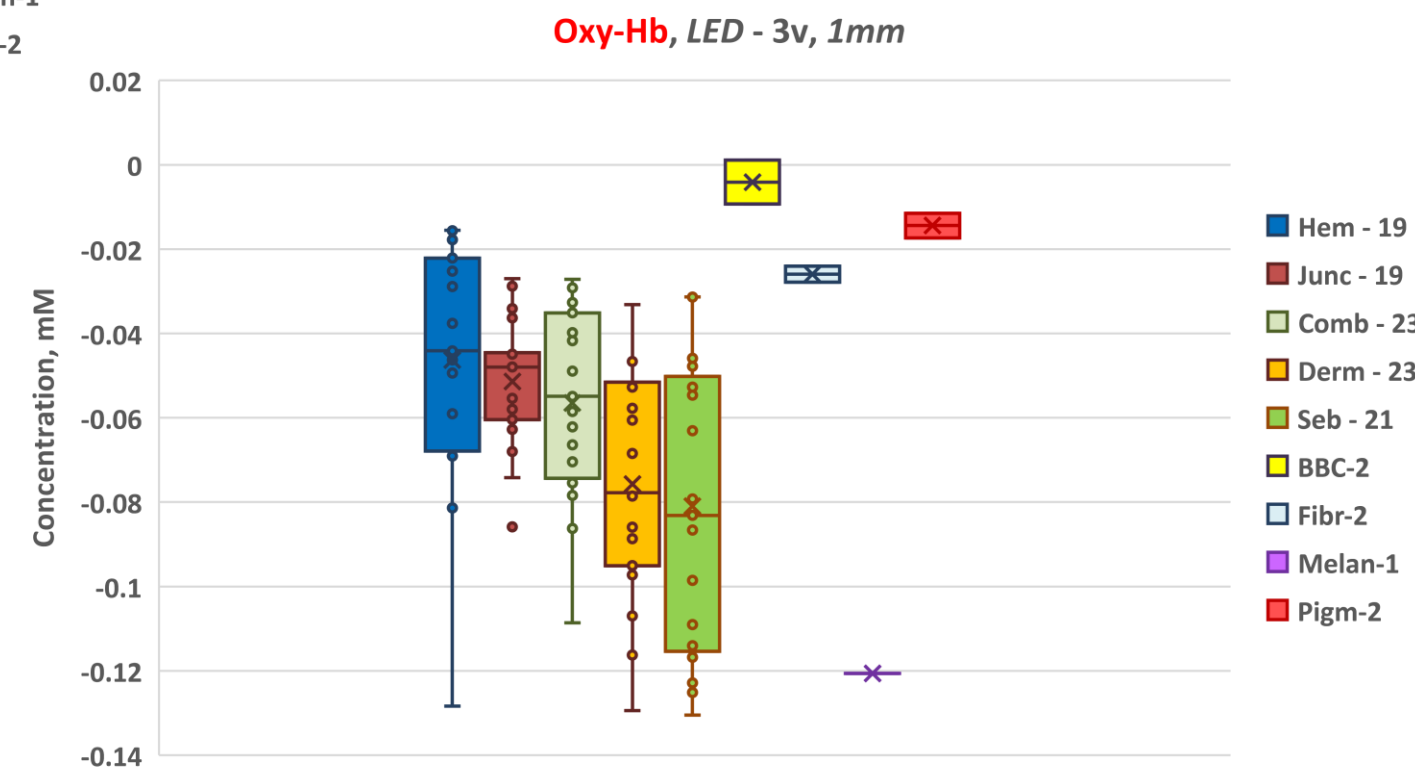
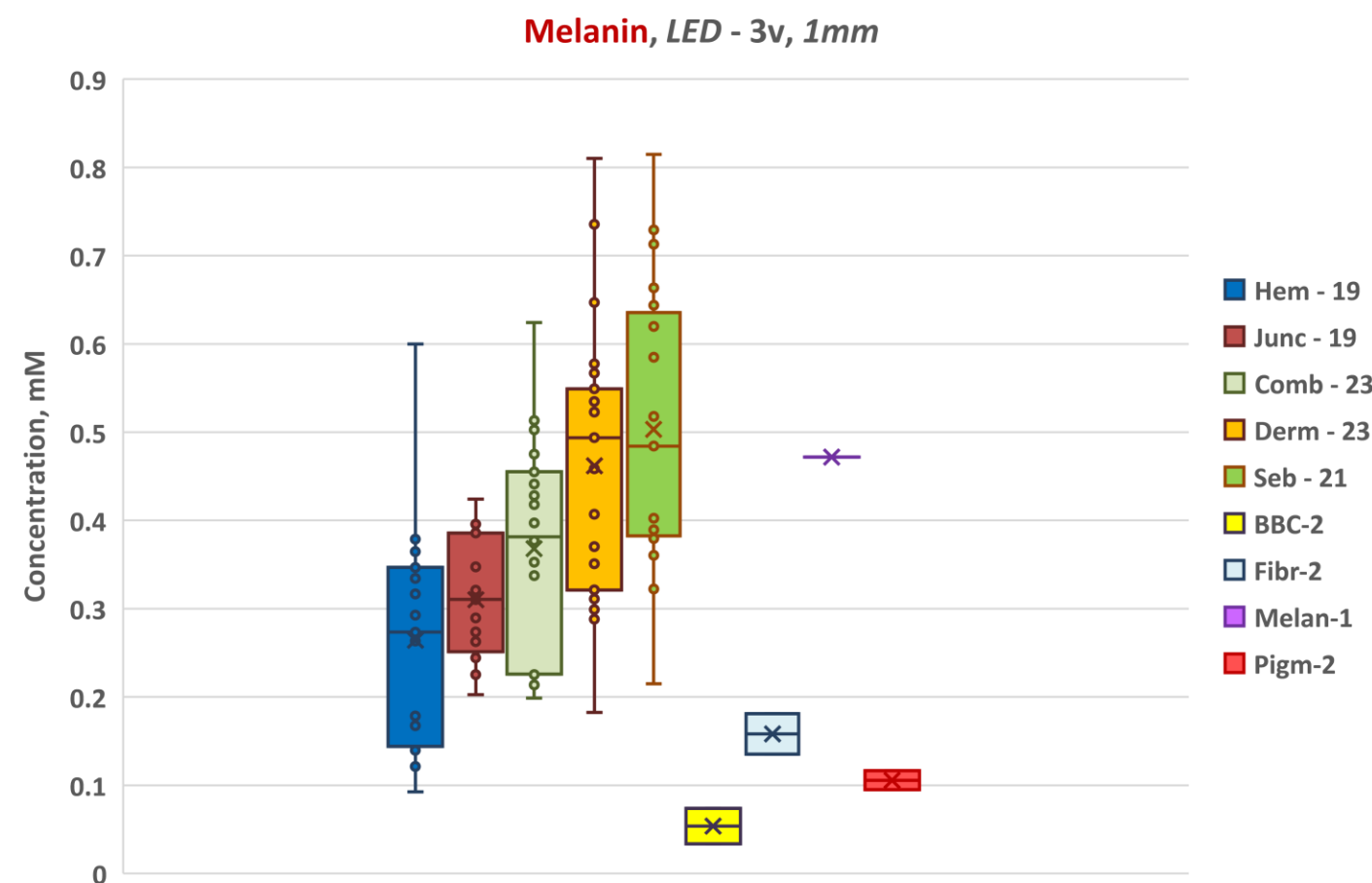




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Third approach for *LED* images



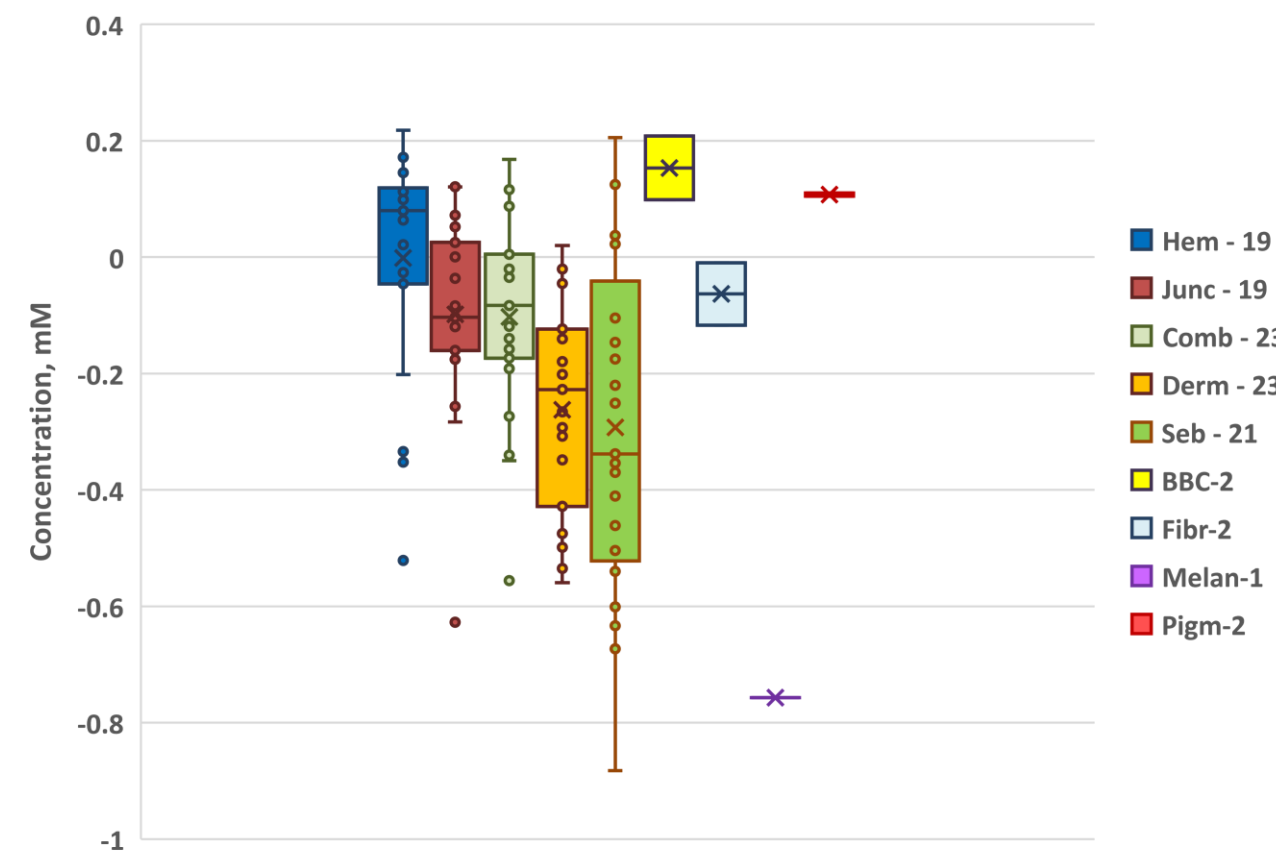


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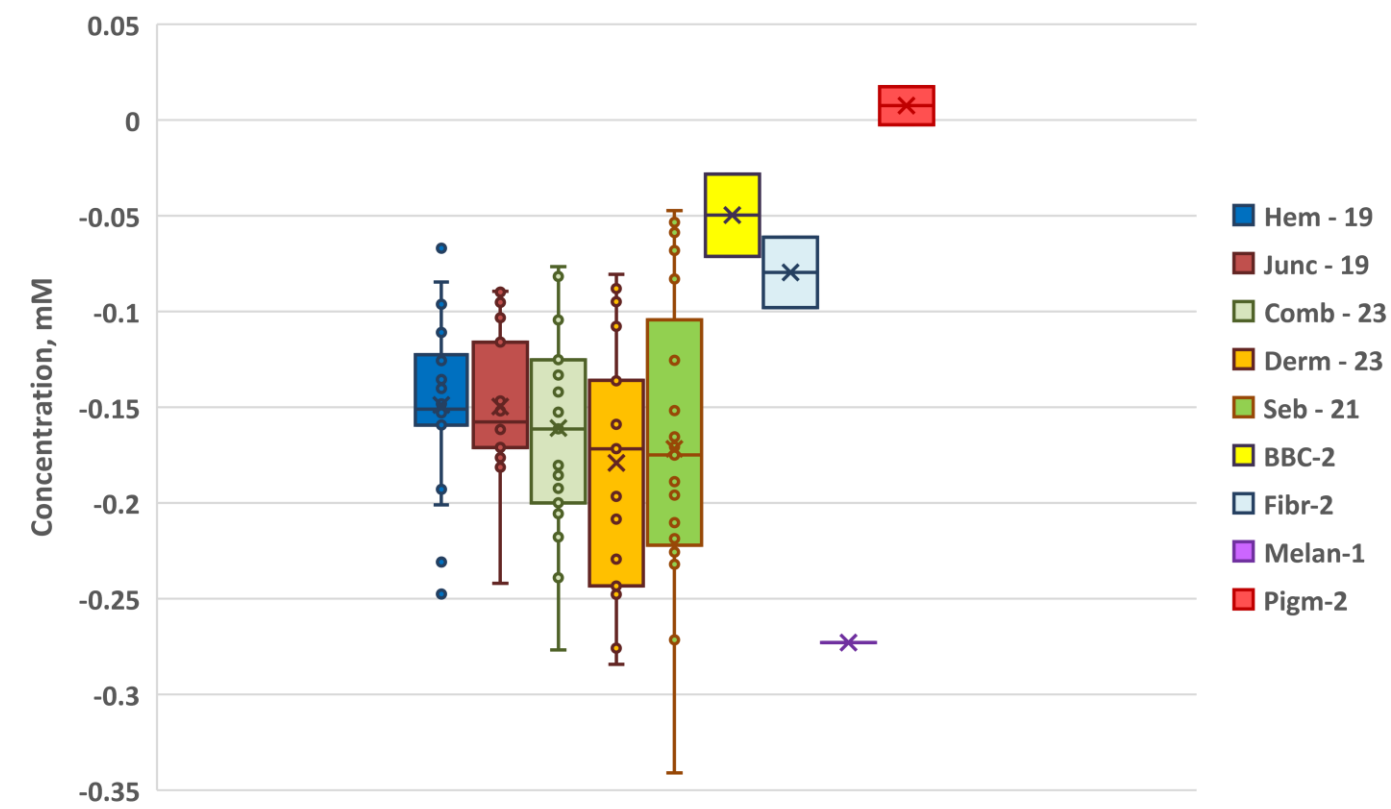
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Third approach for *Laser* images

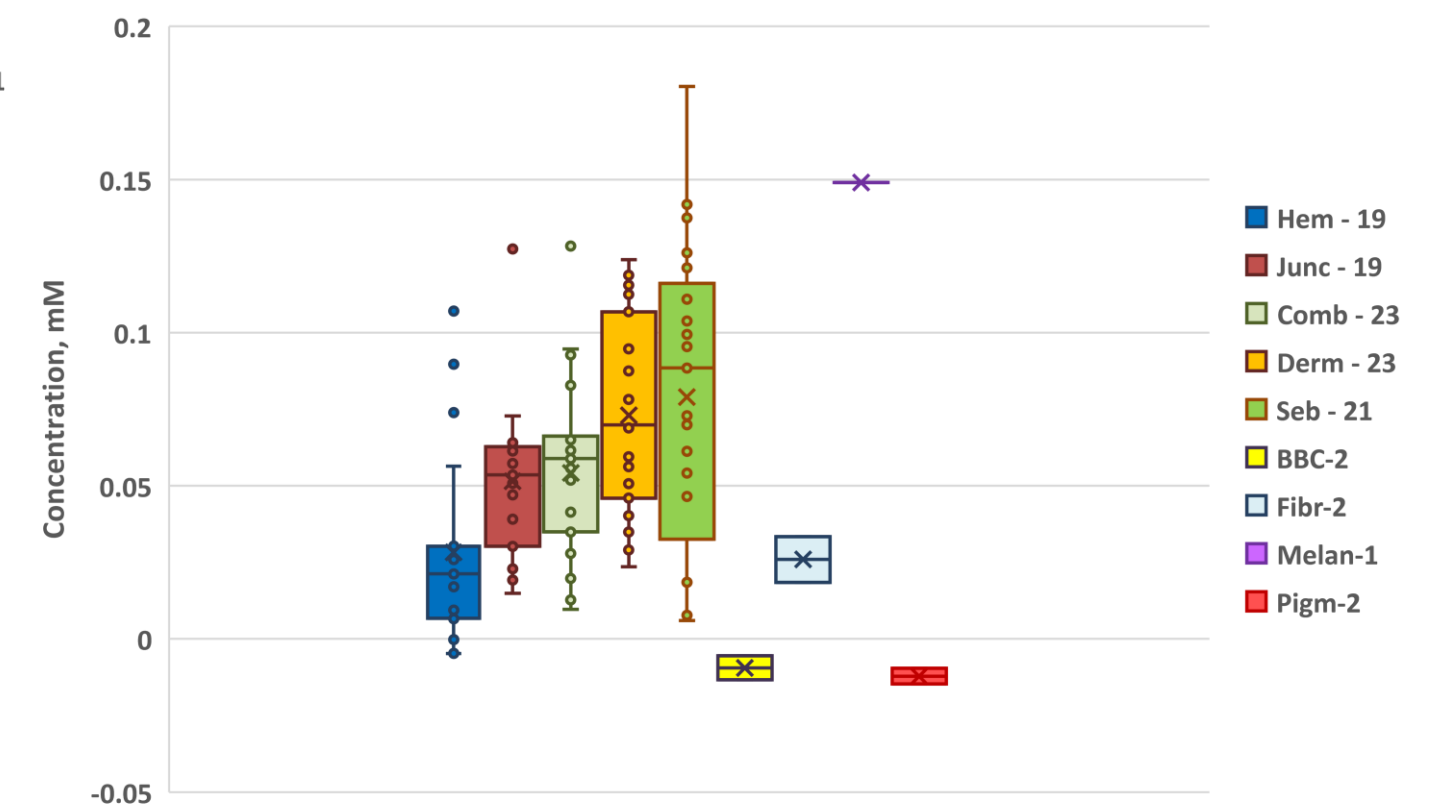
Melanin, *Laser - 3v, 1mm*



Oxy-Hb, *Laser - 3v, 1mm*



Deoxy-Hb, *Laser - 3v, 1mm*

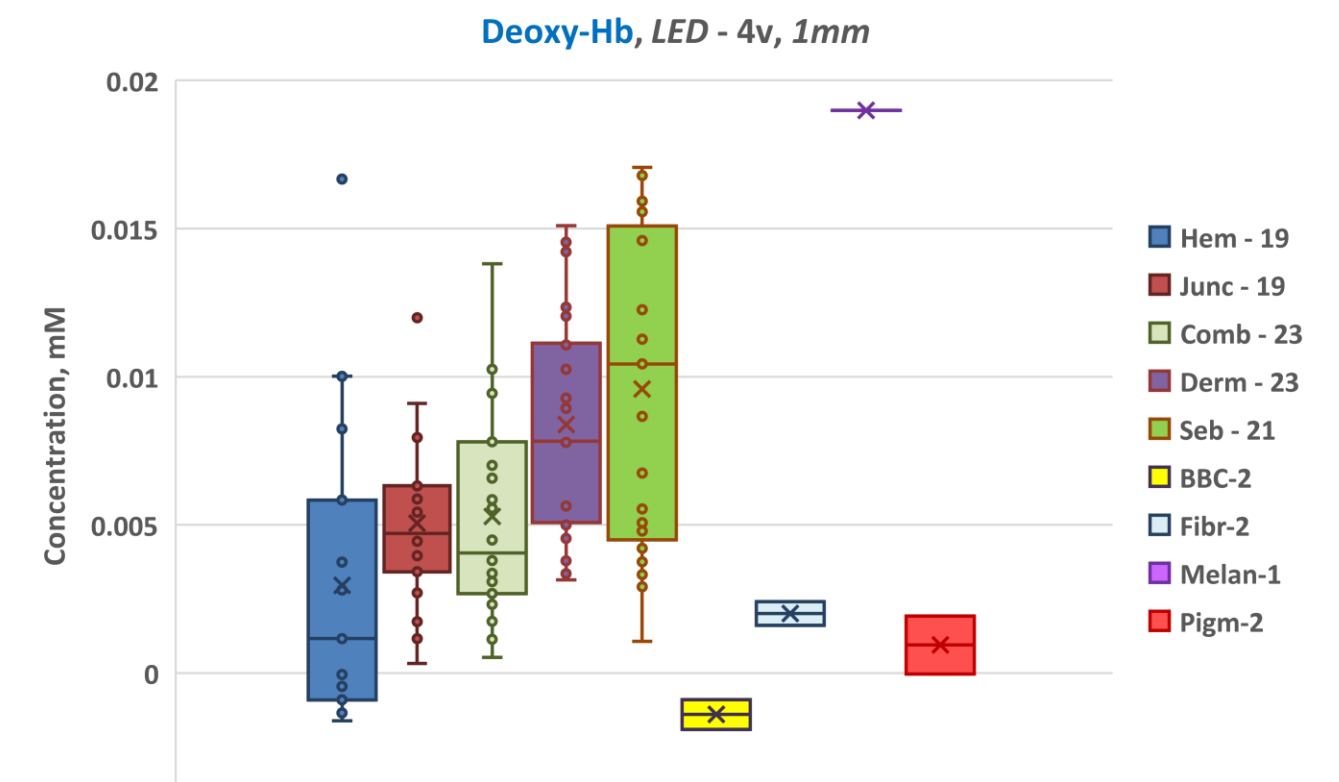
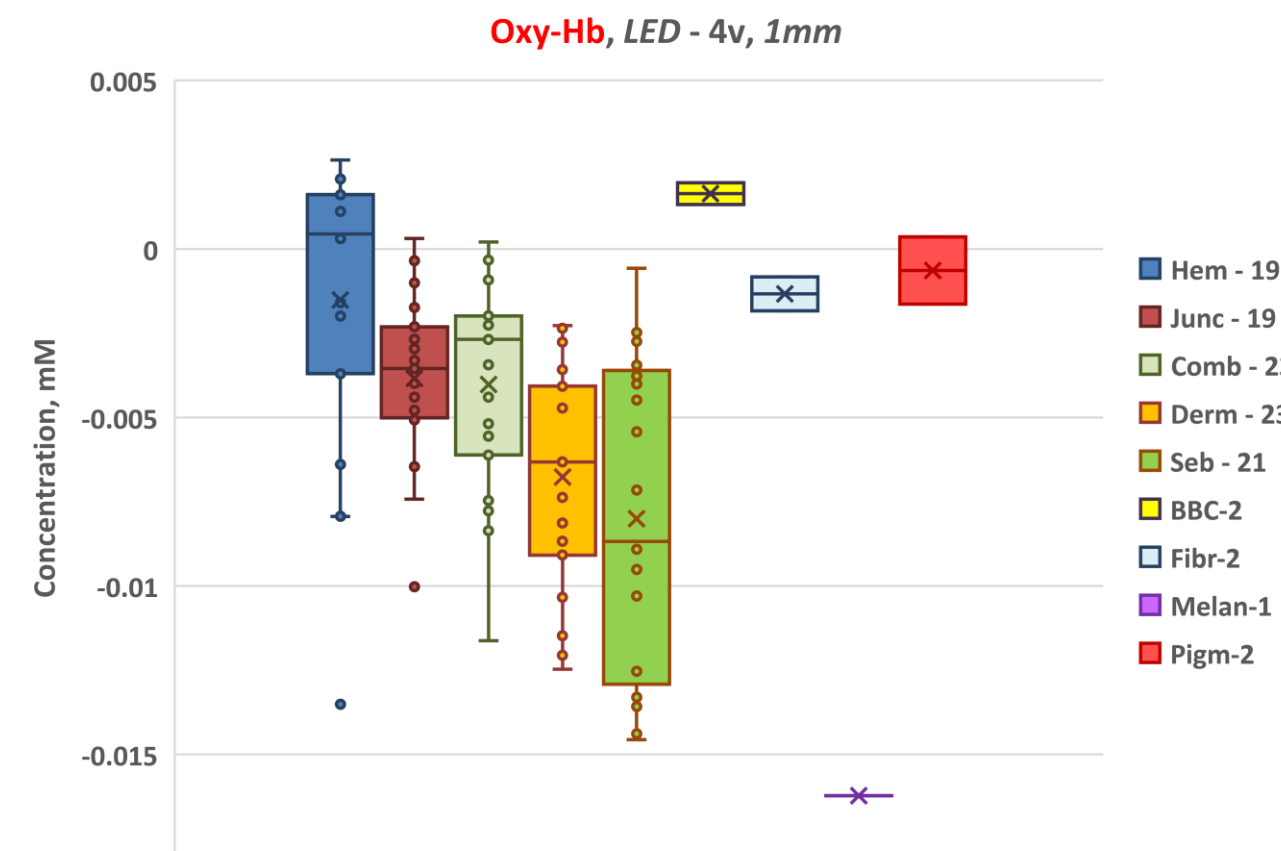
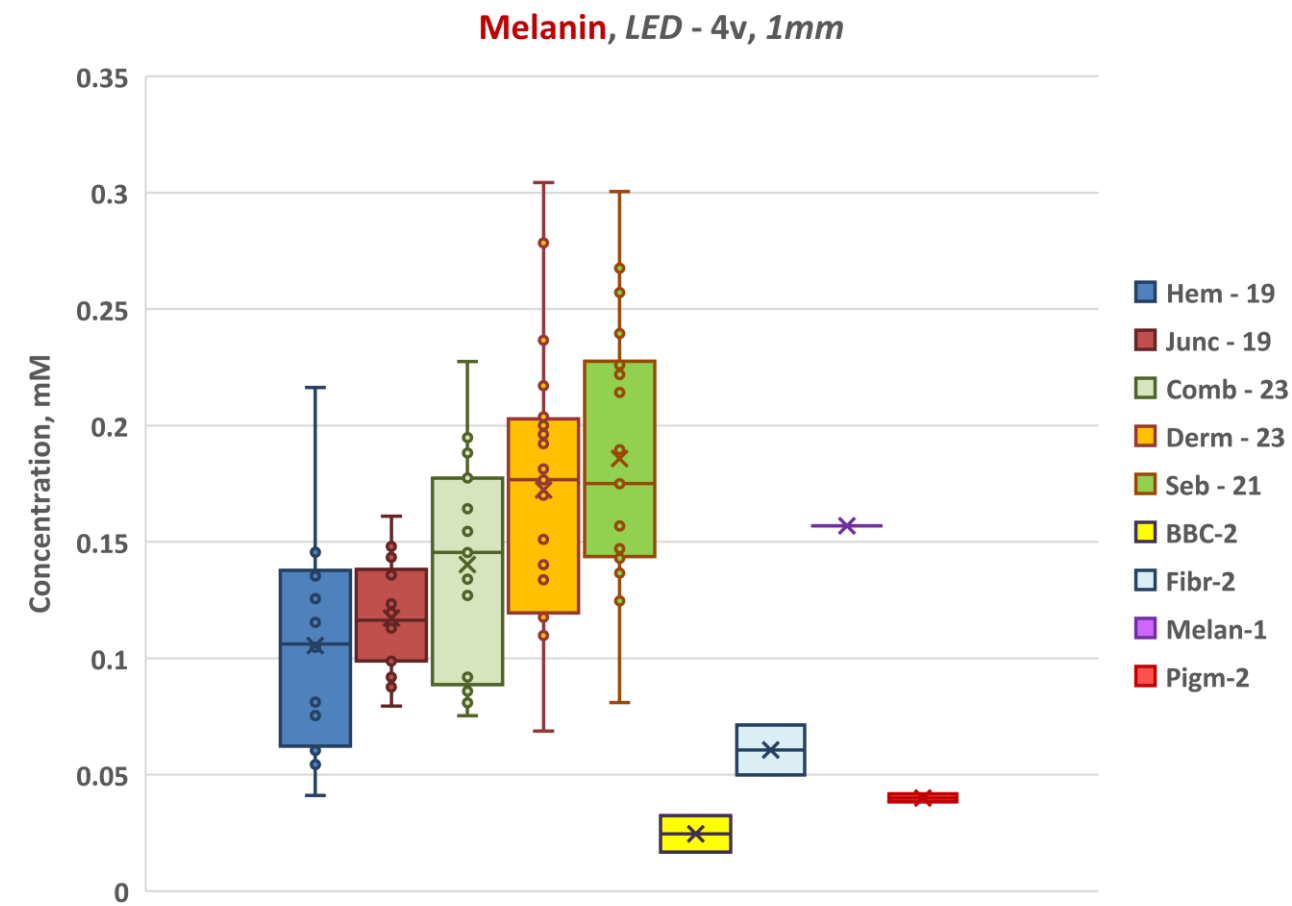




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Fourth approach for *LED* images



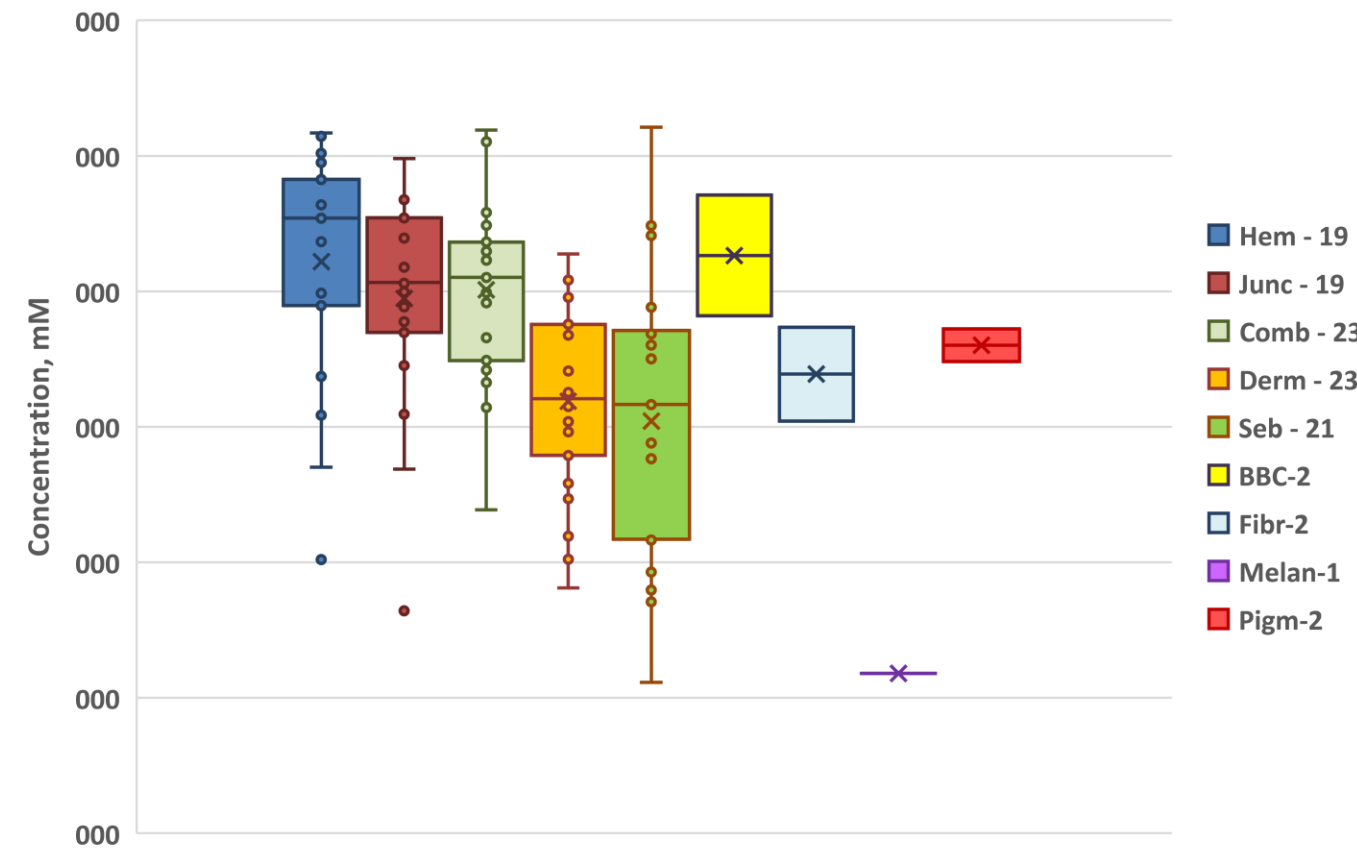


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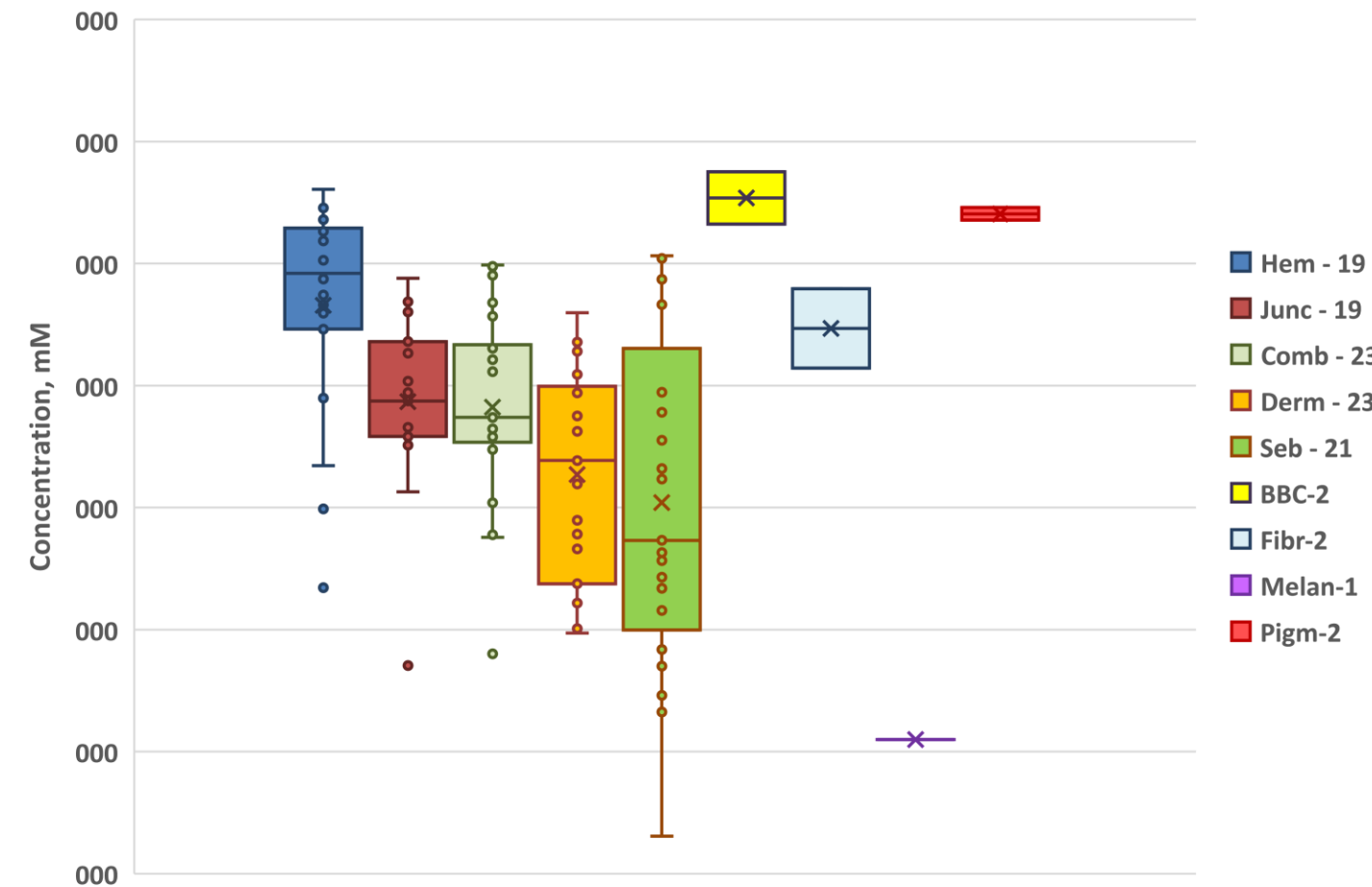
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Fourth approach for *Laser* images

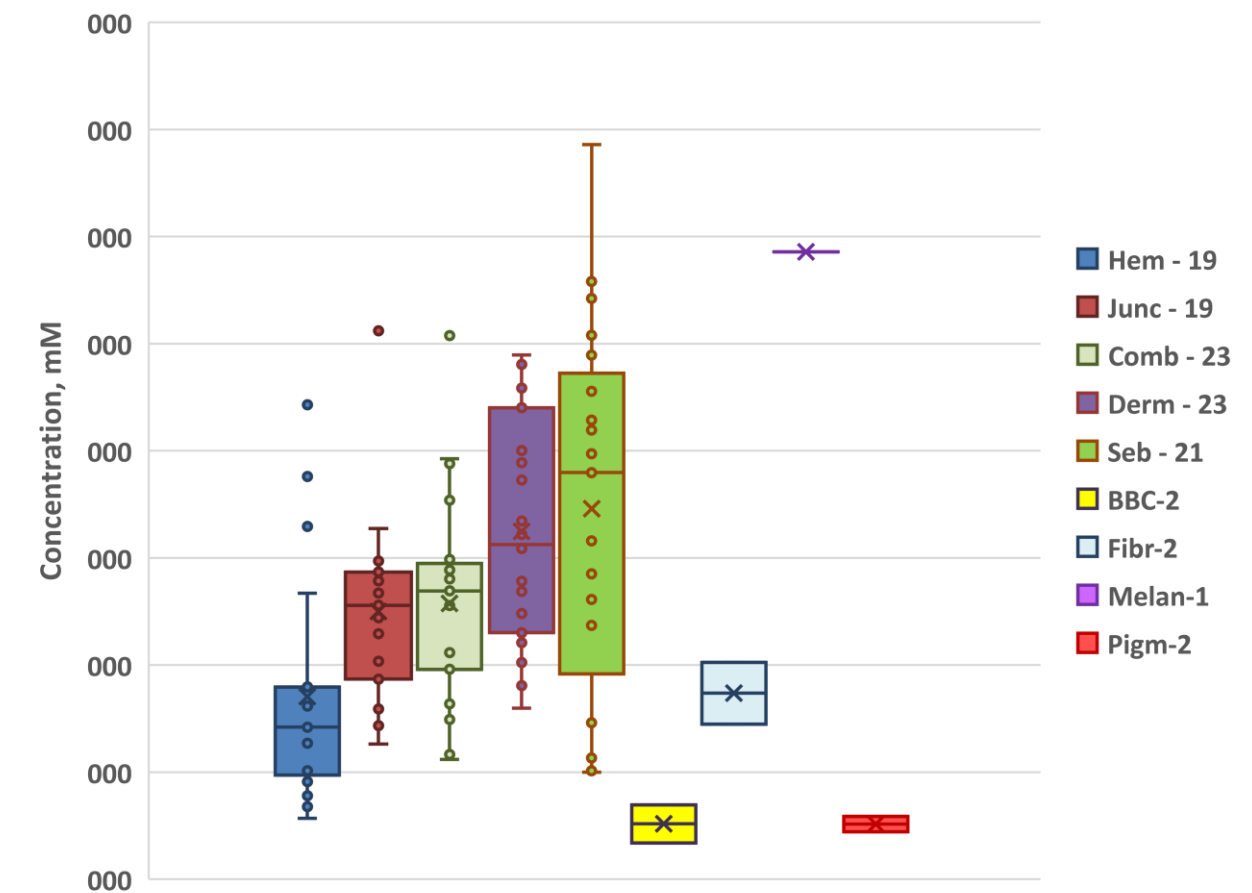
Melanin, Laser - 4v, 1mm



Oxy-Hb, Laser - 4v, 1mm



Deoxy-Hb, Laser - 4v, 1mm





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Conclusion

- The results showed that it is possible to distinguish different types of malformations by comparing the mean values, however the standard deviations overlaps.
- The first approach distinguishes hemangiomas quite well by comparing the hemoglobin and oxyhemoglobin values.
- The third approach showed better results compared to the others due to the largest number of positive concentration values.
- Additional measurements of skin malformations including malignant and suspicious malformations are required for further evaluation of the algorithm.



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Thank you for your attention!



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